

Population pharmacokinetic model of iohexol in dog to estimate glomerular filtration rate and optimize sampling time

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Keywords: dog, Pop PK, iohexol plasma clearance, sampling time optimization, GFR estimation

Abstract

Monitoring iohexol plasma clearance is considered a useful, reliable and sensitive tool to establish glomerular filtration rate (GFR) and early stages of kidney disease in both humans and veterinary medicine. The assessment of GFR based on iohexol plasma clearance needs repeated blood sampling over hours, which is not easily attainable in a clinical setting. Thus, the study aims are to build a population pharmacokinetic (Pop PK) model to estimate iohexol plasma clearance in a population of dogs and based on this model, to indicate the best sampling times that enable a precise clearance estimation using a low number of samples. A Pop PK model was developed based on 5 iohexol plasma samples taken from 5 to 180 minutes (min) after intravenous iohexol nominal dose of 64.7 mg/kg from 49 client-owned dogs of different breeds, sexes, ages, body weights and clinical conditions (healthy or presenting chronic kidney disease CKD). The design of the best sampling times could contain either 1 or 2 or 3 sampling times. These were discretized with a step of 30 min between 30 and 180 min.

A two-compartment Pop PK model best fitted the data, creatinine and kidney status were the covariates included in the model to explain a part of clearance variability. When 1 sample was available, 90 or 120 min were the best sampling times to assess clearance for healthy dogs with a low creatinine value. Whereas for dogs with CKD and medium creatinine value, the best sampling time was 150 or 180 min and for CKD dogs with a high creatinine value 180 min. If 2 or 3 samples were available, several sampling times were possible.

The method to define the best sampling times could be used with other Pop PK models as long as it is representative of the patient population and once the model is built, the use of individualized sampling times for each patient allows to precisely estimate the GFR.

Introduction

Glomerular filtration rate (GFR) is considered the most useful indicator of the overall kidney function and a sensitive biomarker to establish early stages of kidney disease in both humans and veterinary medicine (Schwartz et al. 2006, Lefebvre 2011). In current practice, GFR is generally determined by different methods monitoring plasma clearance of a marker substance, and iohexol is considered a useful and reliable plasma clearance marker (Delanaye et al. 2016b). It is an iodinated non-radiolabeled radiographic contrast agent with low extra-renal excretion, low protein binding, and is neither secreted nor reabsorbed by the kidney (Delanaye et al. 2016a). When used for clearance studies, iohexol has nearly no toxicity and is commercially available at a very low cost. Thus, it has

50 become a key tool to measure GFR (Gaspari et al. 2018, Benz-de Bretagne et al. 2012, Nilsson-Ehle
51 2001) or even a gold standard (Asberg et al. 2020) both in human and in veterinary medicine
52 (Gleadhill and Michell 1996, Heiene and Moe 1998, Finco, Braselton and Cooper 2001, Goy-Thollot
53 et al. 2006, Lippi et al. 2019a, Lippi et al. 2019b, Pocar et al. 2019, Bexfield et al. 2008).

54
55 The assessment of GFR based on iohexol plasma clearance has a major limitation on the requirement
56 of repeated blood sampling over several hours, which is not easily feasible in a clinical setting. Thus,
57 strategies to reduce the number of sampling have been exploited as first reported by Bröchner-
58 Mortensen (1972) in humans. All of these foresaw the addition of correction formulas to achieve
59 more accurate GFR estimation (Gleadhill and Michell 1996, Bexfield et al. 2008, Sasaki et al. 2015,
60 Von Hendy-Willson and Pressler 2011, Pocar et al. 2019). Nevertheless, from veterinary practitioners
61 there is still a demand for reliable and easily applicable GFR estimations methods in a clinical setting.

62
63 Population pharmacokinetics (Pop PK) has been developed to assess the sources of variability of
64 pharmacological agents PK disposition in a target population, and thus to define and estimate the
65 impact of specific factors, such as demographic, pathophysiological, environmental and drug-related
66 (Kiang et al. 2012, Ette and Williams 2004). Additionally, it is able to limit the requirements of
67 sampling designs by applying mixed-effects modeling approaches (Taubert et al. 2018). Moreover,
68 Pop PK approaches are useful to predict a typical PK profile for any given patient when a sufficient
69 knowledge of covariates is available (Concordet, Léger and Ané 2004).

70
71 Starting from recently published data from the same group of authors (Pocar et al. 2019), the first aim
72 of this work was to build a Pop PK model to estimate iohexol plasma clearance for GFR assessment
73 in a population of dogs. Based on this model, the second aim was to indicate the best sampling times
74 that enable a precise clearance estimation using a limited number of samples.

75 **Materials and Methods**

76 **Animals**

77
78 With ethical approval (Organismo Preposto al Benessere Animale, OPBA_107_2016) and after
79 written consent by the owners, 49 client-owned dogs were enrolled for the study. Dogs were of
80 different breeds, sexes, ages, body weights and clinical conditions (healthy or presenting chronic
81 kidney disease, CKD), all scheduled at the University Veterinary Teaching Hospital of the University
82 of Milan for different clinical procedures. A complete physical examination was performed on each
83 dog shortly before GFR evaluation together with complete blood count, serum biochemistry profile
84 and routine urinalysis, UPC ratio and ultrasound examination. According to the guidelines of the
85 International Renal Interest Society (IRIS), dogs were defined as healthy (CKD-, negative) or were
86 diagnosed with chronic kidney disease (CKD+, positive) (Polzin, Osborne and Ross 2005).

87 **Sample collection and analysis**

88
89
90 The whole sampling protocol and analysis were fully described in Pocar et al. (2019). Briefly, iohexol
91 was administered over 60-s periods as intravenous (i.v.) bolus injection via the catheter placed in the
92 left cephalic vein at the nominal dose of 64.7 mg/kg. Blood samples were obtained from the right
93 cephalic vein at 5, 15, 60, 90, and 180 min after administration of the marker, placed in a heparinized
94 tube, and centrifuged to obtain plasma. Samples were stored at -40 °C until extraction and iohexol
95 quantification by validated HPLC method as reported by Pocar et al. (2019). Details on samplings,
96 methods for iohexol determination and GFR estimation described in Pocar et al. (2019) are
97 summarised in Supplementary File 1 (S1).

101 **Population pharmacokinetics**

102

103 Pharmacokinetic modeling was carried out using commercially available software (MONOLIX®
104 version 2018R2, Lixoft, Antony, France). A nonlinear mixed effects (NLME) approach was used to
105 generate Pop PK parameter estimates θ , the interindividual variability Ω and the residual variability
106 σ^2 . One- two- and three-compartment models were evaluated to identify the model that best described
107 the dataset. Model selection was carried out according to different criteria: (i) visual inspection of
108 different diagnostic plot (i.e. visual predictive check, residual plot...), (ii) precision of the estimated
109 parameters, (iii) correct estimation of the information fisher matrix and (iv) values of the objective
110 function (i.e. Likelihood ratio test, LRT; Akaike information criterion, AIC and Bayesian Information
111 Criterion, BIC). The constructed model was of the form:

112

$$113 \begin{cases} \varphi_i = A_i\theta \exp(\eta_i) \text{ where } \eta_i \sim \mathcal{N}(0, \Omega) \\ Y_{ij} = f(t_{ij}; \varphi_i) + g(t_{ij}; \varphi_i; b)\varepsilon_{ij} \text{ where } \varepsilon_{ij} \sim \mathcal{N}(0,1) \end{cases}$$

114

115 Where φ_i is a vector containing individual pharmacokinetic parameters for the i^{th} individual (or its
116 natural logarithm, the vector $\ln\varphi_i$). Y_{ij} is the j^{th} concentration performed on individual i at the moment
117 t_{ij} ; ε_{ij} is the j^{th} residual error for individual i at the moment t_{ij} ; f is a function describing structural
118 model (i.e. it describes concentration evolution over time); g is a function describing residual error
119 model; A_i is a known matrix including covariates of the i^{th} individual; θ is a fixed effects vector
120 including population parameters; Ω is the η_i 's variance-covariance matrix; b is the vector of the
121 parameters involved in the residual error model; and η_i is the vector of the random effects involved
122 in interindividual variability for the i^{th} individual.

123

124 Covariate analysis was performed and the best covariate model was selected based on the decrease
125 of the unexplained interindividual variability, the improvement of the objective function and the
126 absence of precision's loss in the estimated parameters. Nine covariates were tested on individual PK
127 parameters taking into account their plausibility and plots such as individual parameter vs covariates.
128 Weight, age, creatinine, urea and urine specific gravity (USG) were considered as continuous
129 covariates whereas kidney status (healthy: CKD- and diseased: CKD+), gender and breed as
130 categorical covariates. These covariates contain the available information in each dog other than the
131 iohexol concentrations

132

133 **Optimal sampling time**

134

135 Based on the Pop PK model, we looked for the sampling times that allowed the best estimation of
136 iohexol clearance, and therefore the GFR for each dog. These “best sampling” times depend on the
137 available relevant information collected in the dog, i.e. the covariates retained in the final Pop PK
138 model.

139

140 We tried to estimate GFR using 1 single sampling time or 2 or 3 sampling times. These were looked
141 for between 30 and 180 min discretized with a step of 30 min. T1, T2 and T3 were defined as the sets
142 of tested combinations of 1, 2 or 3 times, respectively (i.e. T1={30;...180}; T2={(30, 60); ..., (150,
143 180)}; T3={(30, 60, 90); ..., (120, 150, 180)}).

144

145 The best sampling times change from an individual to another according to the covariates values.
146 Thus, we chose to give three examples of sampling times determination according to the kidney status
147 and creatinine concentration, , defined as follows: (i) CKD- with a creatinine value equal to 0.98
148 mg/dL; (ii) CKD+ with a creatinine value equal to 1.7 mg/dL; (iii) CKD+ with a creatinine value
149 equal to 2.25 mg/dL. These three creatinine values, low, medium and high, were chosen to illustrate
150 the performances of our approach and represent different renal functionality.

151

152 The criterion we chose to compare (and thus select) the different combinations of sampling times was
 153 the Mean Square Error (MSE) for the estimation of GFR. The MSE written as
 154 $MSE = \text{bias}^2 + SD_{\text{imprecision}}^2$ is a kind of proxy statistics that balances the bias and the imprecision of
 155 estimation.

156

157 Using the population parameters previously estimated, 5000 theoretical pharmacokinetic profiles
 158 were simulated for each dog for which the GFR was to be estimated. In other terms, 5000 profiles
 159 were simulated for a combination of covariates A . For a given dog, whose covariates values were
 160 contained in A , the simulated concentrations were obtained using the following model:

161

$$162 \begin{cases} \varphi_i^* = A\hat{\theta} \exp(\eta_i^*) \text{ where } \eta_i^* \sim \mathcal{N}(0, \hat{\Omega}), i = 1, \dots, 5000, \\ Y_{it} = f(t; \varphi_i^*) + g(t; \varphi_i^*; \hat{b}) \varepsilon_{ij}^* \text{ where } \varepsilon_{ij}^* \sim \mathcal{N}(0, 1) \end{cases}$$

163

and $t \in K \subset T1$ or $T2$ or $T3$.

164

165 Then, for each simulated PK profile and each combination K of 1, 2 or 3 sampling times, the
 166 corresponding simulated concentrations were used to predict the GFR. It appeared in the Pop PK
 167 model as a component of φ .

168

169 For a given individual, the Empirical Bayes Estimates (EBE) is a classical predictor of its individual
 170 PK parameters φ . It is obtained as $\hat{\varphi}_K = h(\hat{\eta}_K, \hat{\theta}, A)$ where

171

$$172 \hat{\eta}_K = \text{argsup } P(\eta | Y_K) \quad (\text{Eq.1})$$

173

174 More precisely, if we work on the simulated concentrations $Y_{i,t}^*$

$$175 \hat{\eta}_{i,K}^* = \text{arginf}_{\eta} \sum_{t \in K} \frac{(Y_{i,t}^* - f(t, h(\eta, \hat{\theta}, A)))^2}{g^2(t, h(\eta, \hat{\theta}, A), \hat{b})} + \ln g^2(t, h(\eta, \hat{\theta}, A), \hat{b}) + \eta' \hat{\Omega}^{-1} \eta \quad (\text{Eq.2})$$

176

177 A Gauss Newton algorithm can be used to minimize this equation.

178

179 For the individual for whom the GFR was to be predicted and for a fixed combination of times K , we
 180 computed the 5000 EBE's $(\hat{\eta}_{i,K}^*)_{i=1, \dots, 5000}$ using the simulated concentrations obtained with the same
 181 covariate values as the individual of interest by minimizing Eq. 2. The distance between these EBE's
 182 and the actual η_i^* used to simulate the concentrations gave information on the performances that could
 183 be achieved by estimating the GFR using such a choice of sampling times K . This distance could be
 184 evaluated by the mean square error (MSE) defined as:

185

$$186 MSE_K = \frac{1}{5000} \sqrt{\sum_{i=1}^{5000} (\hat{\eta}_{i,K}^* - \eta_i^*)^2}$$

187

188 MSE_K represented the average distance (in log-scale) between the simulated clearance (i.e. clearance
 189 obtained by Monte Carlo simulations using the Pop PK model) and the estimated clearance. The
 190 combination of times K with the smallest MSE_K were, on average, the best combination of times that
 191 can be used to estimate the GFR of the dog.

192

193 The GFR estimates with EBE were also compared to the GFR obtained by a non-compartmental
 194 approach in the previous paper by Pocar et al. (2019) that consists of computing Dose/AUC/BW
 195 (Supplementary file S1). In this formula, BW is the bodyweight of the animal and AUC is the area
 196 under the iohexol concentration's curve *versus* time. This AUC should be determined from 0 (time of

197 the iohexol administration) to infinity. Because it was expected that no concentrations were small at
198 the last sampling time (180 min), the non-observed part of the curve (post 180 min) was extrapolated
199 to compute the AUC. A Bland-Altman plot was used to compare the results of our approach and the
200 previous one.

201

202 **Results**

203

204 **Animals and iohexol concentrations**

205

206 All animal characteristics are reported in **Table 1** together with the covariates and coding used for
207 Pop PK modeling. Twenty-nine dogs were healthy and 20 diagnosed positive for CKD. The dogs'
208 breeds were heterogeneous, with 10 mongrels and 39 dogs representing 21 different pure breeds. A
209 total of 245 blood samples were taken from all dogs (n. 49) at time intervals of 5, 15, 30, 60, 90 and
210 180 min. The measured iohexol concentrations ranged from 16.4 µg/ml to 643.6 µg/ml. Iohexol
211 plasma concentrations obtained in all 49 dogs are reported in **Figure 1**.

212

213 **Population pharmacokinetics**

214

215 A two-compartment model best fitted the data, as shown in the plots of the observed iohexol
216 concentration versus population predicted concentration or versus individual predicted concentration
217 (**Figure 2**) and in the Visual Predictive Check plot (**Figure 3**). Population value for clearance (θ_{Cl}),
218 central volume of distribution (θ_{V1}), peripheral volume of distribution (θ_{V2}), and intercompartmental
219 clearance θ_Q were estimated and the model included interindividual variability (IIV) on θ_{Cl} , θ_{V1} and
220 θ_{V2} (**Table 2**). The variability error model was best described by a proportional error ϵ (**Table 2**). The
221 value of the residual error was 6.17 %. The correlations between individual parameters were low (<
222 30%) and were therefore not included in the final Pop Pk model.

223

224 Two covariates were included in the final model. They allowed explaining a part of clearance
225 variability. These covariates were centered creatinine value and kidney status defined according to
226 the IRIS score. Covariates were added according to an exponential model. The following equation
227 was used as a covariate model:

228

$$229 \ln(Cl) = \ln(\theta_{Cl}) + \theta_1 * 1_{[diseased\ dogs]} + \theta_2 * ccreatinine\ (mg/dL) + \eta_{Cl}$$

230

231 where $1_{[diseased\ dogs]} = 1$ for dogs with diseased kidney status (CKD+) and 0 for dogs with healthy
232 kidney status (CKD-) and $ccreatinine$ is the creatinine centered around an average value.

233

234 **Optimal sampling time**

235

236 **Figure 4** shows the Bland-Altman plot comparing the GFR obtained by our method to the one
237 obtained by Pocar et al. (2019) when using all the available concentrations. On the x-axis, the means
238 of the two methods are represented (i.e. reference method by Pocar et al. 2019 and our method based
239 on EBE). On the y-axis, the differences between the two methods are shown. The red line depends
240 on the standard error and represents imprecision. The light blue line represents the mean and therefore
241 the bias. The figure shows that the performances of the GFR estimation with the previous and our
242 method are the same when all the available times are used.

243

244 MSE_K results are plotted in **Figure 5** and are summarised in **Tables 3, 4, and 5** for the 3 examples
245 values. The best sampling time depended on the health status and the number of possible samples.
246 When 1 sampling time was available, the best times for clearance calculation were 90 or 120 min for
247 example 1 dogs (CKD- and creatinine value = 0.98 mg/dL), 150 or 180 min for example 2 dogs

248 (CKD+ and creatinine value =1.7 mg/dL), and 180 min for example 3 dogs (CKD+ and creatinine =
249 2.25 mg/dL). When 2 sampling times were available, several sampling times were possible for the 3
250 dog examples. Note that for dogs CKD+ and with high creatinine value (example 3), all the
251 recommended time combinations included sampling at 180 min. When 3 sampling times were
252 available, several times combinations could be envisaged for dogs of examples 2 and 3, whereas for
253 dogs CKD- and with low creatinine value (example 1) all combinations gave similar results, except
254 the combination of the three initial sampling times (30, 60, 90 min).

255

256 **Discussion**

257

258 To the author's knowledge, this is the first study that builds a Pop PK model to estimate iohexol
259 plasma clearance in a population of dogs and by the model, an innovative approach is reported to
260 choose the best sampling time to precisely estimate iohexol clearance and therefore GFR with a
261 reduced number of samples. The study is innovative and useful, considering the constant demand for
262 reliable and easily applicable GFR estimations methods by veterinary practitioners. Nevertheless, the
263 approach and model here reported could be considered a "model" for studies in other species and
264 humans.

265

266 No other studies report a Pop PK model to estimate clearance and GFR in dogs, but in humans a
267 recent study by Taubert et al. (2018), reports a Pop PK model using a three-compartmental model to
268 better estimate iohexol clearance. These authors support the existence of a third compartment where
269 iohexol rapidly distributes soon after administration and affects the whole concentration-time curve.
270 More recently, Asberg et al. (2020) reported a Pop PK method to determine iohexol clearance in
271 humans using a two-compartment model.

272

273 Similarly, the PK parameters of iohexol in dogs were best described by a two-compartment model
274 with a linear elimination. The different sampling times of our study (till 180 min vs 300 min by
275 Taubert et al. 2018) can have influenced the detection of a third compartment, so as the old age of the
276 patients (>70 years) in Taubert et al.'s (2018) study. Moreover, to support our model, the
277 interindividual variability was around 20 % on all the parameters except intercompartmental
278 clearance that was fixed. Furthermore, all parameters in the model were precisely estimated with
279 percent relative standard errors < 15 % for the fixed effect and < 30 % for the standard deviation of
280 the random effects (**Table 2**). None of the goodness-of-fit plots showed a systematic bias or trend.
281 The intraindividual variability was around 6 %, which is small enough to expect precise Bayesian
282 estimations.

283

284 The robustness of the results was strengthened by the inclusion of a varied population of dogs both
285 by their demographical characteristics and by their renal status. Indeed, dogs' weights ranged from
286 3.9 kg to 46 kg. The values of creatinine and urea varied respectively from 0.67 to 14.4 mg/dL and
287 from 16 to 181.4 mg/dL. Finally, female, male and female neutered dogs were included in the study
288 allowing to study a sex-effect. Furthermore, the Pop PK parameters' estimates were consistent with
289 the data published in our previous work (Pocar et al., 2019) and this supports the reliability of our
290 Pop PK model.

291

292 Covariate analysis was performed to identify the influence of various baseline characteristics on the
293 PK of iohexol. Two covariates explained a part of the variability of iohexol elimination clearance:
294 plasma creatinine and kidney status (CKD- or +). The creatinine value as a major covariate was not
295 surprising as both creatinine and iohexol are eliminated by glomerular filtration. The kidney status
296 (CKD- or +) that takes into account creatinine value and different clinical and biological variables
297 was also a significant covariate of iohexol elimination clearance. Urea could have been an interesting

298 covariate as its elimination mechanism is mainly by glomerular filtration. Nevertheless, in this study,
299 it did not appear to explain a part of the elimination clearance variability of iohexol and this could be
300 explained by two reasons. On one hand, urea is less specific than creatinine to indicate kidney disease
301 (Finco and Duncan, 1976). On the other hand, the part of variability on the elimination clearance
302 explained by urea is the same as the one explained by creatinine. Thus, urea appears as a covariate
303 only in the absence of data on creatinine.

304
305 Otherwise, the covariate analysis did not reveal the influence of any breed or age on the iohexol PK.
306 Physiologically, age was expected to be a significant covariate due to the progressive decrease of the
307 glomerular filtration rate with age. However, here it did not appear as an influential covariate probably
308 because the age can not be interpreted without breed or body size (Kraus et al., 2013). To put in
309 evidence an effect of age, we should have related age to life expectancy. Moreover, the breeds
310 represented in this study were too heterogeneous (mongrels and 21 different pure breeds) to influence
311 the model.

312
313 To cope with the need for reliable and feasible GFR estimation methods in the clinical practice, we
314 looked for a method to reduce the number of necessary samples to precisely estimate iohexol
315 clearance, and therefore the GFR, in order to promote its use in the clinics. It was not the definition
316 of an optimal design, which, by definition, requires as many sampling times as the number of
317 individual PK parameters to estimate. Therefore, after obtaining the model, we studied a methodology
318 to obtain the best sampling times to allow a correct estimation of the iohexol clearance. This
319 methodology was different from the previous methodology already published that used D optimality
320 and Ds optimality criterion (Mentré et al., 1997; Tod et al. 1998; Fedorov, 2013). Indeed, these criteria
321 focused on determining the best sampling times that minimize the asymptotic evaluation of
322 imprecision of the individual clearance. This approach is relevant when the number of blood sampling
323 performed in the individual under investigation is large. Differently, we wanted to estimate
324 parameters with a maximum of 3 blood samples, but our estimate could be both biased (eta-shrinkage)
325 and imprecise. This was the reason why we used the MSE that combines both imprecision (variance)
326 and bias, and indicates how close the estimator is to the true value (Walther and Moore, 2005).

327
328 Elimination clearance was larger in dogs CKD- and with low creatinine value (example 1) than in
329 dogs CKD+ (examples 2 and 3). It was thus expected that the best 1-sampling time for animals CKD-
330 and with low creatinine value (example 1) was earlier than the one for the other animals. In fact, in
331 our study when experimental design with 1 sampling was considered, the best sampling times were
332 90 or 120 min for dogs CKD- with low creatinine value (example 1) and 180 min for dogs CKD+
333 with the high creatinine value (example 3). Surprisingly, the optimal sampling time for dogs with
334 creatinine value equal to 1.7 mg/dL was the same as for dogs with a creatinine value equal to 2.25
335 mg/dL (150 or 180 min). It was probably because the last sampling time (180 min) was too early for
336 sick dogs. In fact, all dogs CKD+ with the high creatinine value had an iohexol concentration greater
337 than 100 µg/mL at 180 min. These concentration values represented more than 50 % of the peak
338 concentration (taken 5 min after the injection) except for one dog for which the 180 min concentration
339 represented 20 % of the 5 min concentration. These results showed that the elimination was not ended
340 and that the real optimal experimental design might include times later than 180 min for the sick dogs.
341 These results could also call into question the quality of the parameters estimates provided by the
342 model, especially clearance, but this was not the case, because the distribution of iohexol is very rapid
343 since it diffuses freely through membranes due to its chemical properties. It has been demonstrated
344 that in CKD+ dogs the slope of the iohexol plasma decay curve decreases at three hours (180 min)
345 leading to the formation of an excretion plateau (Lippi et al., 2008). The same authors observed that
346 estimated GFR based on a sampling protocol ending at 180 min shows better correlation with real
347 GFR than protocols including later timing (e.g. 300 or 420 min). Finally, single sampling protocols
348 at 180 min for GFR estimation have been demonstrated to have an acceptable error margin for both

349 healthy and sick dogs (Pocar et al., 2019). Considering the clinical practice, it is important to have a
350 reliable evaluation of iohexol clearance and consequently GFR as soon as possible and within a
351 reasonable time when patients are in the hospital. Thus, although iohexol elimination has not ended,
352 a 180 min sampling time is a useful tool to help the clinicians in detecting kidney disease resulting in
353 the best compromise between the accuracy of GRF estimation and the time advantage for the dog and
354 owner.

355
356 When 2 or 3 sampling times were considered, for the dogs CKD+ with medium or high creatinine
357 values (example 2 and 3), the best results were obtained from the combination of times including
358 times far from the administration, as also observed in human transplanted patients, where the optimal
359 combination of time points included concentrations measured at the extreme times (120 and 270 min)
360 (Benz de-Bretagne et al. 2012). For dogs CKD- and with low creatinine value, the results were more
361 smoothed and many combination times could be considered especially with 3 sampling times, where
362 all except the first can be considered. For these dogs, MSE was not improved when 1, 2 or 3 sampling
363 times were considered, thus, 1 well-chosen sampling time is sufficient to precisely estimate clearance
364 and taking other samples is not necessary. The same observation can be done also for dogs CKD+
365 and medium or high creatinine values, as, also for these dogs, MSE did not change when combining
366 1, 2 or 3 sampling times. In summary, before estimating GFR in a dog using iohexol, knowing the
367 creatinine value is essential to choose the best sampling time and to limit costs and save time. Then,
368 the methods to further estimate GFR based on iohexol clearance and limited sampling times can
369 follow the different steps reported by Pocar et al. (2019).

370
371 The method to define the best sampling times could be used with other Pop PK models as long as the
372 model is correctly built, includes covariates to limit the interindividual variability and presents a weak
373 value for the intraindividual variability.

374
375 The limited number of dogs in this study may have had an impact on our results for three main
376 reasons: 1) The sample size is directly linked to the representativeness of the sample and thus to the
377 possibility to extrapolate the results to other dogs. As already mentioned, the aim of this article was
378 to use all available and relevant information in a dog to estimate its GFR. We found that plasma
379 creatinine and renal status based on IRIS score gave information on GFR, but it is not clear if the
380 relationship between GFR and the creatinine/renal status is the same for all dog breeds. A study with
381 only 49 dogs cannot be representative of all dogs breeds, as there exist more than 300 dog breeds.
382 Thus, a study with several thousands of dogs would be necessary to properly document this.

383 2) The sample size is also limited for the validation of the Pop PK model. While we strictly validated
384 the model according to the recommendations given in the best PK journals for Pop PK model
385 validation, we agree, in view of point 1) that this sample size is not large enough for a population
386 validation. We rely on the results given for the breeds represented in this study, but we cannot exclude
387 that these results would be approximate for other breeds. 3) The article wants to propose a
388 methodology to choose the best sampling times to estimate a dog GFR according to the information
389 available in this dog. The sampling times were chosen so that the MSE was minimal. The sample size
390 has a direct influence on the imprecision of the MSE ($MSE = bias^2 + SD_{\text{imprecision}}^2$) estimation; that is,
391 on the bias and imprecision estimation. To our knowledge, no methods are allowing to estimate *a*
392 *priori* (before having any preliminary results) the sample size for bias and imprecision estimation in
393 such models. The best published results on this topic (Mentré et al., 1997, Tod et al. 1998, Fedorov
394 2013, Mentré et al., 2013) are asymptotic (one assumes that the sample size is infinite) and require
395 precise knowledge of the model parameters. Even if the sample size is important for the MSE
396 estimation, the "optimal sampling" times obtained with an imprecise MSE can be expected to be close
397 to the one that would be obtained with larger sample size.

398

399 Finally, this work supports a global approach of personalized medicine and its application in human
 400 medicine or other veterinary species can be possible, like for example in cats. Cats are low compliant
 401 patients and reducing sampling numbers can greatly reduce the animal stress and could make the GFR
 402 procedure reasonably feasible in the clinical practice. The only prerequisite of this methodology is to
 403 obtain data sufficiently reliable to build a Pop PK model representative of the patient population.
 404 Once the model is built, the use of individualized sampling times for each patient allows estimating
 405 with precision the GFR.

406 **Author Contributions**

407 PP, PS, VB and PC designed the trial and conducted the experimental phase; SB and DC conducted
 408 Pop PK analysis and optimal sampling time definition; PC and SB drafted the paper. All the co-
 409 authors critically reviewed several drafts and approved the final manuscript.

410 **Conflict of Interest Statement**

411 The authors declare that the research was conducted in the absence of any commercial or financial
 412 relationships that could be construed as a potential conflict of interest.

413 **Tables**

414 **TABLE 1: Animal characteristics, covariates and coding used in Pop PK analysis**

Continuous covariates			
	Mean ± S.D.	range (median)	
Age (y)	5.43 ± 3.5	0.4-16 (4.5)	
Body weight (kg)	25.8 ± 9.5	3.9-46 (27.6)	
Serum creatinine (mg/dL)	1.47 ± 1.99	0.67-14.4 (1.09)	
Serum Urea (mg/dL)	44.95 ± 34.81	16-181.4 (36)	
Urine specific gravity (USG)	1036.78 ± 18.59	1003-1065 (1040)	
Categorical covariates			
	Type and number of subjects (Code)		
Renal status (Chronic Kidney Disease, CKD)	Healthy CKD- n = 29 (Code 0)	Diseased CKD+ n = 20 (Code 1)	
Breed	Mongrel n = 10 (Code 0)	Other breeds n = 39 (Code 1)	
Sex	Male n = 19 (Code 0)	Female n = 6 (Code 1)	Female neutered n = 24 (Code 2)

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TABLE 2: Synthesis of estimates obtained in the final Pop PK model.

Parameters	Units	Value	SE	RSE (%)
θ_{cl}	L/min/kg	0.00212	0.00010	4.68
θ_{v1}	L/kg	0.163	0.00661	4.07
θ_{v2}	L/kg	0.058	0.00387	6.64
θ_Q	L/min/kg	0.0034	0.00042	12.21
Covariates				
θ_1 (diseased dogs)		-0.379	0.07002	18.49
θ_2 (creatinine)	dL/mg	-0.421	0.05356	12.72
Variability				
η_{cl}		0.208	0.02255	10.85
η_{v1}		0.248	0.02718	10.95
η_{v2}		0.199	0.05618	28.21
Residual error				
ε		0.0617		

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TABLE 3: Mean square error for the time combination K (MSE_K) results of optimal designs including 1 sample (TC: Time Combination). The best sampling times for each example of dogs are in red.

		Example 1 (CKD- and creatinine value = 0.98 mg/dL) ($\times 10^{-3}$)	Example 2 (CKD+ and creatinine value = 1.7 mg/dL) ($\times 10^{-3}$)	Example 3 (CKD+ and creatinine value = 2.25 mg/dL) ($\times 10^{-3}$)
TC	1 Sampling time	MSE	MSE	MSE
1	30	2.37144	2.83923	2.87982
2	60	1.48213	2.49541	2.71283
3	90	1.08587	2.06094	2.33112
4	120	1.04398	1.55052	2.03204
5	150	1.15137	1.21796	1.58001
6	180	1.27023	1.05704	1.27007

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TABLE 4: Mean square error for the time combination K (MSE_K) results of optimal designs including 2 samples (TC: Times Combination). The best sampling times for each example of dogs are in red.

		Example 1 (CKD- and creatinine value = 0.98 mg/dL) ($\times 10^{-3}$)	Example 2 (CKD+ and creatinine value = 1.7 mg/dL) ($\times 10^{-3}$)	Example 3 (CKD+ and creatinine value = 2.25 mg/dL) ($\times 10^{-3}$)
TC	2 sampling times (min)	MSE	MSE	MSE
1	30_60	1.59044	2.94597	3.38164
2	30_90	1.04184	2.02553	2.47435
3	30_120	0.8313	1.52744	1.88487
4	30_150	0.77656	1.24404	1.54674
5	30_180	0.76386	1.04572	1.29145
6	60_90	1.01744	2.11078	2.63993
7	60_120	0.8628	1.53112	1.91978
8	60_150	0.84146	1.18311	1.49829
9	60_180	0.83782	1.00331	1.21676
10	90_120	0.90116	1.65281	2.14052
11	90_150	0.89505	1.23837	1.6483
12	90_180	0.91048	1.00323	1.29749
13	120_150	0.99535	1.22089	1.67092
14	120_180	1.00764	0.9865	1.34951
15	150_180	1.17352	0.97719	1.24635

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TABLE 5: Mean square error for the time combination K (MSE_K) results of optimal designs including 3 samples (TC: Times Combination). The best sampling times for each example of dogs are in red.

		Example 1 (CKD- and creatinine value = 0.98 mg/dL) ($\times 10^{-3}$)	Example 2 (CKD+ and creatinine value = 1.7 mg/dL) ($\times 10^{-3}$)	Example 3 (CKD+ and creatinine value = 2.25 mg/dL) ($\times 10^{-3}$)
TC	3 sampling times (min)	MSE	MSE	MSE
1	30_60_90	1.01127	2.00212	2.43594
2	30_60_120	0.79361	1.49464	1.81317
3	30_60_150	0.72799	1.20321	1.48077
4	30_60_180	0.68501	0.98346	1.22154
5	30_90_120	0.75675	1.43671	1.80194
6	30_90_150	0.69878	1.17373	1.45919
7	30_90_180	0.67861	0.97652	1.2322
8	30_120_150	0.68581	1.09122	1.38739
9	30_120_180	0.67313	0.93237	1.18603
10	30_150_180	0.67858	0.8623	1.10814
11	60_90_120	0.79057	1.47998	1.86321
12	60_90_150	0.75929	1.1665	1.50283
13	60_90_180	0.75331	0.96534	1.23779
14	60_120_150	0.76469	1.07649	1.396
15	60_120_180	0.75608	0.9122	1.16991
16	60_150_180	0.77419	0.84264	1.08415
17	90_120_150	0.82071	1.14447	1.55208
18	90_120_180	0.81691	0.94613	1.2775
19	90_150_180	0.86003	0.88547	1.18735
20	120_150_180	0.95395	0.884564	1.23236

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450 **Supplementary Material**

451 **Supplementary file S1:** description of sampling protocol, iohexol analytical method and GFR
452 estimation as reported in the previous paper by Pocar et al. (2019).

453

454 **Figures**

455 **Figure 1:** Semi-logarithmic spaghetti plots of iohexol plasma concentrations over 180 min after a
456 single i.v. administration (nominal dose of 64.7 mg/kg) in 49 dogs

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458 **Figure 2:** Plots of the observed iohexol concentration ($\mu\text{g/mL}$) versus population predicted
459 concentration (left) or versus individual predicted concentration (right). The points are distributed
460 homogeneously around the identity line showing the model well described the data.

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462 **Figure 3:** Visual Predictive Check (VPC) plot was obtained with empirical data (blue lines) and
463 simulated data. Multiple Monte Carlo simulations allowed defining theoretical percentiles (10^{th} , 50^{th}
464 and 90^{th}) and their prediction interval. Empirical and theoretical percentiles are superposed showing
465 that the model well described the data.

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467 **Figure 4:** Bland-Altman plot of the comparison of GFR obtained with the formula $\text{Cl}=\text{D}/\text{AUC}$ in the
468 previously published paper by Pocar et al. (2019) and Empirical Bayes Estimates (EBE) (5 sampling
469 times available).

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471 **Figure 5:** Plots of mean square error for the time combination K (MSE_K) versus time for the 3 dog
472 examples (CKD- and low creatinine value, CKD+ and medium creatinine value and CKD+ and high
473 creatinine) when 1, 2 or 3 samples were available (respectively, left, middle, and right).

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