Introduction

Per oral endoscopic myotomy (POEM) and endoscopic submucosal dissection (ESD) are well-established techniques in GI endoscopy [1–3]. These procedures are possible by means of electrosurgical devices able to transform high frequency alternate electrical current into thermal energy for either ablation, coagulation or cutting purposes [4]. At the current state of the art, thermal energy is conveyed within the tissue by direct contact of conductive electrosurgical probes in both POEM and ESD [1, 2]. In standard endoscopic settings, electrosurgical accessories are safely employed in many clinical applications, also including hemostasis, tissue ablation and tumor debulking, with rare complications. However, the thermal energy delivered by conductive probes within the tissue may provoke lateral and transmural injuries (≥2–3 mm) and eventually bleeding and perforation. Such complications depend on many factors including duration of application, power settings, rate and mag-
ntitude of electrosurgical current, tissue resistance and probe properties. Accordingly, prolonged administration of thermal energy onto the same area is not generally advisable [4]. Nonetheless, in challenging endoscopic tasks, such as ESD and POEM, the extensive and sustained use of electrosurgical devices may account for a certain burden of complications [4].

The Thulium-doped yttrium-aluminium-garnet laser system (TLS), a recently developed therapeutic laser, earns a chance to overcome these limitations. The TLS acts with a continuous or pulsed wave mode at 2.0-μm (▶ Fig. 1) [5]. Already employed in surgery and endourology, this new laser technique has gained rapid consensus among specialists as a reliable therapeutic tool for surgical resection, vaporesection, ablation, and coagulation, thus substituting less precise laser techniques (e.g., Holmium laser) [6–11]. To our knowledge, the experience on the use of the TLS in GI endoscopy is very limited [12, 13].

In this study, we evaluated for the first time the feasibility of TLS-assisted gastric ESD and POEM in standard experimental models assessing the laser-induced tissue damage to the submucosal and muscle layer.

Materials and methods

All procedures were conducted ex vivo in an established experimental setting by using two porcine models of the upper GI tract. The TLS applied during this study was the Cyber TM® (Quanta System SpA, Varese, Italy) (▶ Table 1). This laser system acts with a 2.0-μm wavelength providing a wide range of power settings (1–200 W) suitable for both surgical and endoscopic uses [8–13]. For the purposes of the present study, we evaluated power settings ranging from 5 to 30 W emitted with either a continued or a pulsed laser configuration. Various flexible optical fibers (272 and 365 μm-thick) were also tested.

Two Western endoscopists were involved, 1 with substantial skills in either gastric ESD (40–50 procedures) or POEM (20–30 procedures), and 1 with no expertise with these techniques. Both operators had very limited previous experience on the ex vivo use of this new endoscopic device. All procedures were conducted using standard high-definition gastroscopes and digitally recorded.

The ESD of 3 large (mean 3.5 cm, range 3.3–3.6 cm) injection-induced (saline solution) lesions of the stomach was performed following a standard technique in two ex vivo models. The TLS-guided POEM was simulated performing an esophageal incision and submucosal tunnelling down to the gastroesophageal junction in 2 ex vivo models.

Following the endoscopic procedures, an expert gastrointestinal pathologist performed the histopathological analysis on the entire stomachs looking for signs of transmural perfora-
tion or tissue injuries affecting the *muscularis propria* or the deepest submucosal layer.

**Results**

Complete en bloc gastric ESD was feasible in all cases. Both endoscopists reported an easy maneuverability regardless of their expertise in ESD procedures ([Video 1](https://www.thieme-connect.com/DOI/DOI?10.1055/s-0043-106738)). ESD operative time ranged between 30 and 70 minutes according to the operator’s expertise in ESD as well as in TLS-assisted ESD ([Table 2](#)). More in detail, 10 to 30 minutes were needed for gastric mucosal incision, and 20 to 40 minutes for gastric lesions dissection.

The lesions’ border was traced using a 5-W laser output. The 272-µm and the 365-µm thick optical fibers appeared equally effective for both mucosal incision and submucosal dissection using various power settings (20–35 W for incision, 15–25 W for dissection). A progressive increase in the favorite power setting was observed for both operators over the course of their performance: the best-perceived power output turned from 20 W to 25 to 30 W for mucosal incision and from 15 to 20 W for submucosal dissection. Laser emission in continuous mode resulted in clearer cutting lines and was adopted by both operators instead of the pulse modality.

Excessive smoke, albeit never obscuring the endoscopic view, was observed during mucosal incisions when laser emission was used in air on dry tissue ([Fig. 2](#)). On the contrary, smoke emission was largely less when submucosal dissection was done. Histopathology performed on the gastric wall corresponding to the 3e ESD treatments confirmed the absence of transmural perforation, thereby showing no tissue damage within the *muscularis propria* and the deepest submucosal layer ([Fig. 3](#)).

Both esophageal incisions and submucosal tunneling down to the gastroesophageal junction were also feasible within 20 to 30 minutes and regardless of the operators’ expertise ([Video 2](https://www.thieme-connect.com/DOI/DOI?10.1055/s-0043-106738), [Fig. 4](#)). Even in this setting, the 272-µm and 365-µm thick optical fibers appeared equally effective for both mucosal incision and submucosal tunneling using various power settings (20–35 W for incision, 15–25 W for dissection). The best-perceived power setting was 25 W for mucosal incision and 15–20 W for submucosal tunneling, operating in continuous mode. As for gastric ESD, smoke emission was evident yet non-influential during mucosal incision and negligible during submucosal tunneling.

As confirmed by histopathology, no transmural perforation, neither to the luminal side (i.e., mucosal) occurred ([Table 2](#), [Fig. 5](#)).

<table>
<thead>
<tr>
<th>Operator</th>
<th>Dimension</th>
<th>Time</th>
<th>Outcomes</th>
</tr>
</thead>
<tbody>
<tr>
<td>ESD No. 1</td>
<td>1</td>
<td>3.6 cm</td>
<td>50 minutes</td>
</tr>
<tr>
<td>ESD No. 2</td>
<td>1</td>
<td>3.3 cm</td>
<td>30 minutes</td>
</tr>
<tr>
<td>ESD No. 3</td>
<td>2</td>
<td>3.5 cm</td>
<td>70 minutes</td>
</tr>
<tr>
<td>POEM No. 1</td>
<td>1</td>
<td>–</td>
<td>20 minutes</td>
</tr>
<tr>
<td>POEM No. 2</td>
<td>2</td>
<td>–</td>
<td>30 minutes</td>
</tr>
</tbody>
</table>

Operator No.1 – Expert gastrointestinal endoscopist with initial expertise in ESD and POEM.
Operator No.2 – Expert gastrointestinal endoscopist with no previous experience in ESD and POEM.

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**Table 2** ESD and POEMs specifications.

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**Video 1:** Thulium-assisted endoscopic submucosal dissection in *ex vivo* porcine model.

**Video 2:** Thulium-assisted per oral endoscopic myotomy in *ex vivo* porcine model.

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Discussion

Previous surgical and endourological in vivo studies demonstrated how laser technology may be considered an effective and successful alternative to standard electrosurgical devices [5–8]. Recently, we evaluated the potential of the TLS in GI endoscopy. The TLS provided favorable performance in ex vivo models as compared to argon plasma coagulation and was successfully adopted for the endoscopic treatment of non-variceal upper GI bleeding in vivo [13]. In particular, the 2.0-μm wavelength of the TLS allows a very confined vaporesective and hemostatic effect on the targeted mucosal surface, reducing the chance of unexpected injuries on the underlying tissue [13].

Another pilot study conducted in vivo showed that the Thulium laser is a feasible tool for ESD in early gastric epithelial neoplasia. In that paper from Korea, curative resection was achieved in 9/10 patients without relevant complications. All procedures were performed by a single very experienced endoscopist (>1000 ESD); nonetheless, authors reported a prolonged incision time to avoid accidental deep tissue injuries [12]. We therefore conducted a feasibility study in ex vivo models to evaluate the effect of TLS-assisted ESD on deeper gastric layers and to test its performance even in less expert hands (<50 ESD).

This study confirms both the feasibility and safety of TLS in performing ESD and POEM. Either mucosal incision and submucosal dissection or submucosal tunneling were easily performed regardless of the operator’s expertise. The use of this non-contact device for mucosal incision and submucosal dissection allowed the endoscopists to easily assess the conditions of the digestive wall in real time, while operating throughout all the procedure, thereby reducing the risk of unnoticed deep tissue injuries. Consistently, histopathological analysis on the entire upper gastrointestinal models revealed that TLS has no impact on the deeper layers during ESD and POEM.

These initial results support future implementations of laser-assisted techniques for advanced endoscopic treatments. In
particular, the use of incision devices with very confined impact on deeper layers and high hemostatic efficacy can potentially improve both technical and clinical outcomes associated with ESD and POEM, especially when bleeding or severe fibrosis with muscle fibers adherent to the submucosal layer increase the risk of perforation [14, 15]. Peculiar benefits of the TLS beyond additional laser systems include a continuous wave mode combined with the highest coefficient of absorption in water, meaning more precise cutting power and a higher hemostatic potential. On the contrary, the Holmium laser provides a pulsed wave mode at 2.1 μm, therefore inducing deeper coagulation on soft tissue (▶Fig. 1) [7,13].

Another matter associated with the use of laser systems for surgical purposes relies on the optical fibers durability. Optical fibers with limited duration show a progressive depletion of laser collimation, thereby spreading the laser beam on a less limited and symmetric target. On the contrary, we never changed the two probes (272 and 365 μm thick) during this study. Experiences from laser enucleation of the prostate showed that the TLS optical fibers maintain similar performance during prolonged uses (up to 60 minutes under continuous emission in water immersion) with very high-power settings (> 100W) [9]. In addition, the TLS reusable optical fibers recover their original performance just cleaving the terminal 1 cm of the tip (using a dedicated ceramic blade) following several and prolonged uses. All reusable TLS optical fibers can be sterilized (e.g., steam and gas-plasma sterilization). To date, there is no study assessing the cumulative use (in term of operative time or power output) associated with a significant reduction of the TLS optical fiber performances. Consistently, there is no standardized limit beyond which a revision of the optical laser tip is recommended. Based on our experience, additional variables might also interfere with this correlation, such as their use in air versus liquid, probe overheating and previous contact of the optical fiber tip with organic tissues.

Remarkably, smoke emission and evacuation could represent an issue for prolonged TLS use in air, especially on dry tissue and during mucosal incision either for in vivo [12] or ex vivo settings [13]. In our experience, both water irrigation through the ancillary working channel of the endoscope and lasing in water immersion were smoke-free procedures. In fact, no accessory device assisting the use of frontal optical fibers during endoscopic laser treatments has been planned so far (e.g., for irrigation, injection, smoke evacuation, rotation, orientation). To date, needle-knife or paintbrush like laser emissions can be delivered only straight on the optical fiber placed at the tip of the endoscope’s working channel.

These aspects together with the very limited operators’ experience with use of this novel endoscopic tool may have played a role in determining the wide range of time to achieve a complete gastric ESD within this ex vivo study. The use of bloodless experimental settings usually results in shorter operative time. On the contrary, the observed ESD operative time of 30 to 70 minutes is in line with those observed for in vivo TLS-assisted ESD of 1 to 2 cm gastric epithelial neoplasia reported by Cho J-H et al. (median 49 minutes, range 35 – 2013 minutes) [12]. However, the second TLS-assisted ESD performed by the same operator was much quicker than the previous one in our study, thereby suggesting a substantial learning curve effect related to the use of this novel endoscopic tool for ESD.

Notably, the TLS wavelength of 2 μm has an innate hemostatic effect and has already shown promising performance when adopted to treat ongoing bleedings in vivo [5 – 13]. Accordingly, the main limitation of this feasibility study relies on its bloodless experimental setting, which could have been not appropriate to highlight one of the potential key features of this technique, which is a more potent hemostatic effect.
Conclusion

In conclusion, our ex vivo experiences suggest that TLS is a precise and manageable endoscopic treatment device. By means of different optical fibers and power settings, the TLS appears perfectly suitable for several and heterogeneous endoscopic treatments, including ESD and POEM. Nonetheless, we advocate the need of in vivo preliminary assessment to confirm our ex vivo results. Should these results be replicated, large prospective trials will be required to assess the opportunity of adding TLS to endoscopists’ toolbox.

Acknowledgments

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Competing interests

G.C. is currently employed at the Surgical Division of Quanta System. The remaining authors disclosed no financial relationships relevant to this publication.

References