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2 **Low non-carbonic buffer power amplifies acute respiratory acid-base disorders**
3 **in septic patients: an *in-vitro* study**

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22 **Running head:** Non-carbonic buffer power in sepsis

23

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27

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29 TL conceived the study, collected, interpreted and analyzed data, searched literature, and wrote the
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45

46 **Abstract**

47 **Rationale:** Septic patients have typically reduced concentrations of hemoglobin and albumin, the
48 major components of non-carbonic buffer power (β). This could expose patients to high pH
49 variations during acid-base disorders.

50 **Objectives:** To compare, *in-vitro*, non-carbonic β of septic patients with that of healthy volunteers,
51 and evaluate its distinct components.

52 **Methods:** Whole blood and isolated plasma of 18 septic patients and 18 controls were equilibrated
53 with different CO₂ mixtures. Blood gases, pH and electrolytes were measured. Non-carbonic β and
54 non-carbonic β due to variations in Strong Ion Difference (β_{SID}) were calculated for whole blood.
55 Non-carbonic β and non-carbonic β normalized for albumin concentrations (β_{NORM}) were calculated
56 for isolated plasma. Representative values at pH=7.40 were compared. Albumin proteoforms were
57 evaluated via two-dimensional electrophoresis.

58 **Measurements and Main Results:** Hemoglobin and albumin concentrations were significantly
59 lower in septic patients. Septic patients had lower non-carbonic β both of whole blood (22.0±1.9 vs.
60 31.6±2.1 mmol/L, p<0.01) and plasma (0.5±1.0 vs. 3.7±0.8 mmol/L, p<0.01). Non-carbonic β_{SID}
61 was lower in patients (16.8±1.9 vs. 24.4±1.9 mmol/L, p<0.01) and strongly correlated with
62 hemoglobin concentration (r=0.94, p<0.01). Non-carbonic β_{NORM} was lower in patients (0.01 [-0.01
63 – 0.04] vs. 0.08 [0.06 – 0.09] mmol/g, p <0.01). Septic patients and controls showed different
64 amounts of albumin proteoforms.

65 **Conclusions:** Septic patients are exposed to higher pH variations for any given change in CO₂ due
66 to lower concentrations of non-carbonic buffers and, possibly, an altered buffering function of
67 albumin. In both septic patients and healthy controls, electrolyte shifts are the major buffering
68 mechanism during respiratory acid-base disorders.

69

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71 **Keywords:** Sepsis; Acid-Base Equilibrium; Acidosis, Respiratory; Buffers; Electrolytes.

72 **New & Noteworthy (67/75)**

73 Septic patients are poorly protected against acute respiratory acid-base derangements due to a lower non-
74 carbonic buffer power, which is caused both by a reduction in the major non-carbonic buffers, *i.e.*
75 hemoglobin and albumin, and by a reduced buffering capacity of albumin. Electrolyte shifts from and to the
76 red blood cells determining acute variations in Strong Ion Difference are the major buffering mechanism
77 during acute respiratory acid-base disorders.

78

79 **Introduction**

80 Sepsis is a life-threatening disease leading worldwide to 5 million yearly deaths (1, 2). Metabolic
81 acidosis is common in sepsis and is a marker of severity (3, 4). Furthermore, about 40% of septic
82 patients develop secondary respiratory failure and are therefore at risk of respiratory acidosis (5, 6).

83 In human physiology, two systems limit pH changes in acute acid-base perturbations: the
84 carbonic (carbonic acid/bicarbonate) and non-carbonic buffers (mainly albumin and phosphates in
85 plasma, with the addition of hemoglobin in whole blood) (7).

86 Both systems contribute to the acute compensation of metabolic derangements, *e.g.* in case of lactic
87 acidosis both bicarbonate ions (HCO_3^-) and the dissociated part of non-carbonic buffers (A^-) will be
88 reduced. On the contrary, during acute respiratory acid-base derangements only non-carbonic
89 buffers minimize pH variations, as the change in carbonic acid/bicarbonate is the primary disorder
90 (8). In this context, the ability of non-carbonic buffers to limit pH excursions has been termed as
91 non-carbonic buffer power (β) and defined as the negative value of the variation in HCO_3^- divided
92 by the corresponding variation in pH, induced by acute changes in partial pressure of carbon
93 dioxide (PCO_2) (7, 9-11). Simplifying, this means that, for any given variation in PCO_2 , a patient
94 with a lower non-carbonic β will have greater pH variations as compared to a patient with higher
95 values of non-carbonic β .

96 In order to effectively buffer respiratory acid-base derangements, and limit pH variations,
97 non-carbonic buffers have to favor changes in HCO_3^- consensual to the variations in PCO_2 .
98 According to the electrical neutrality principle, the total concentration of cations has to be equal to
99 the total concentration of anions (12, 13). As a direct consequence, any increase in HCO_3^- observed
100 during acute hypercapnia must be accompanied by a reduction in negative charges and/or an
101 increase in positive charges. This can be achieved in two ways. First, through a reduction in the
102 dissociated part of total non-carbonic weak acids (A^-), such as proteins and phosphates, therefore

103 operating in the buffer base domain (14-16). Second, through a reduction in strong anions, mainly
104 chloride (Cl⁻) or an increase in strong cations, mainly sodium (Na⁺), therefore operating in the
105 Strong Ion Difference (SID) domain (12, 17, 18). The first mechanism is considered the main in
106 isolated plasma. On the other hand, when dealing with a complex solution, such as whole blood, red
107 blood cells gain a key role as they allow electrolytes shifts across their cellular membrane, leading
108 to SID changes consensual to PCO₂ variations (8, 19, 20).

109 During sepsis, patients are typically anemic (21) and hypoalbuminemic (22, 23), and have
110 therefore reduced concentrations of non-carbonic buffers. Moreover, albumin is a macromolecule
111 whose structure might vary significantly (24). Indeed, pathological conditions such as inflammation
112 might favor the transition from reduced albumin to “oxidized” albumin (25). If and how these
113 changes of protein structure might affect its buffering function is currently unknown.

114 As data regarding the non-carbonic β of septic patients are currently lacking, we decided to
115 conduct this prospective, experimental *in-vitro* acid-base study. We hypothesized that septic
116 patients’ non-carbonic β of whole blood and plasma would be significantly lower as compared to
117 healthy volunteers, thus exposing patients to greater pH variations.

118

119 **Materials and Methods**

120 *Study population*

121 The study was approved by the ethical committee and registered at ClinicalTrials.gov
122 (NCT03503214). Patients admitted to the intensive care unit for sepsis/septic shock (3) were
123 enrolled. Age < 18 years and pregnancy were exclusion criteria. Healthy, age-matched volunteers
124 were recruited for comparison. Informed or deferred informed consent was obtained.

125

126 *Blood and plasma sample*

127 In both groups, 25 milliliters of venous blood were collected (26, 27). Complete blood count,
128 concentrations of magnesium, phosphate and albumin (Cobas c-702, Roche, Switzerland) were
129 measured. Six milliliters were placed in anti-foam syringes (T310 Syringes, RNA Medical, USA),
130 *i.e.* plastic syringes pre-treated with an anti-foam material in order to prevent excessive foaming
131 during tonometry. The remaining blood was centrifuged for 10 minutes at 4°C at 3000 rpm to
132 isolate plasma. A sample was frozen at -85°C for subsequent biomolecular analyses.

133

134 *Tonometry of blood and plasma*

135 The whole blood sample was divided in four aliquots and immediately equilibrated at different CO₂
136 concentrations through tonometry (Equilibrator, RNA Medical, USA) (27-29). Four gas mixtures
137 containing 2, 5, 12 or 20% of CO₂ with 21% of oxygen and nitrogen for the remaining percentage
138 were used (15 minutes at 37°C). Thereafter, samples were analyzed for blood gases, pH and
139 concentrations of sodium, potassium, calcium, chloride and lactate (ABL 800 FLEX Radiometer,
140 Denmark). Samples in which lactate increased more than 1 mmol/L as compared to baseline values,
141 and samples in which hemoglobin saturation for oxygen was below 94% were discarded. The same
142 procedure was performed on isolated plasma.

143 *Definitions and calculations*

144 For each whole blood sample the actual SID obtained at every CO₂ concentration was calculated as:

$$145 \quad [\text{SID}] = [\text{Na}^+] + [\text{K}^+] + 2 \times [\text{Ca}^{2+}] - [\text{Cl}^-] - [\text{lactate}^-] \quad [1]$$

146 where Na⁺, K⁺, Ca²⁺, Cl⁻ and Lactate⁻ refer to plasma sodium, potassium, ionized calcium, chloride
 147 and lactate concentrations (expressed in mmol/L) measured with the point-of-care blood gas
 148 analyzer. Magnesium was not used for the calculation, as it was measured only in the central
 149 laboratory on baseline venous blood. The actual HCO₃⁻ concentration of each sample was calculated
 150 by applying known values for the solubility of CO₂ in plasma (S = 0.0307 mmol/(L·mm Hg)) (30)
 151 and the negative logarithm of the first apparent equilibrium dissociation constant of carbonic acid
 152 (pK'₁ = 6.095 for whole blood and pK'₁ = 6.105 for isolated plasma) (31):

$$153 \quad [\text{HCO}_3^-] = S \cdot \text{PCO}_2 \cdot 10^{(\text{pH} - \text{pK}'_1)} \quad [2]$$

154 where PCO₂ = partial pressure of carbon dioxide (expressed in mm Hg) and measured with the
 155 point-of-care blood gas analyzer and pH = pH measured with the point-of-care blood gas analyzer.

156 Variations of HCO₃⁻ and SID over pH in whole blood and plasma were modeled according to a
 157 polynomial multilevel model (32) in order to obtain overall HCO₃⁻/pH and SID/pH curves for the
 158 two study groups and individual best fits for all subjects/patients.

159 Non-carbonic β was defined as -ΔHCO₃⁻/ΔpH resulting from a variation in PCO₂ (7). Non-carbonic
 160 β is therefore the opposite of the first derivative of the HCO₃⁻/pH curve:

$$161 \quad \text{Non-carbonic } \beta = -d[\text{HCO}_3^-]/dpH \quad [3]$$

162 Individual non-carbonic β curves were used to obtain representative non-carbonic β values
 163 at a pH of 7.40 (β_{7.40}).

164 The same analysis was performed substituting SID to HCO₃⁻ in order to quantify the contribution of
 165 the electrolyte shifts to total non-carbonic β in whole blood:

$$166 \quad \beta_{\text{SID}} = -d\text{SID}/d\text{pH} \quad [4]$$

167 Individual values of non-carbonic β of isolated plasma obtained at pH=7.40 were divided by the
168 albumin concentration in order to normalize for different albumin concentrations and investigate the
169 molecular buffering function:

$$170 \quad \beta_{\text{NORM}} = \beta_{7.40}/\text{Albumin [g/L]} \quad [5]$$

171

172 *Polynomial multilevel model*

173 Variations of dependent variables over pH were modeled according to a polynomial multilevel
174 model (general linear mixed models) with random intercept at subject level and random slope at pH
175 level. Statistical analyses were performed as previously described (29) and carried out by SAS 9.4
176 statistical package. The exponential power of pH was decided according to model-based likelihood
177 ratio tests (cut-off P-value ≤ 0.100). Interaction between the independent variables, pH
178 and subjects' group (controls and patients), was also included according to model-based likelihood
179 ratio tests.

180

181 *Two-dimensional electrophoresis (2-DE)*

182 Total proteins in plasma samples were quantified and separated by two-dimensional electrophoresis
183 (2-DE). The total protein content in plasma samples was assessed by the bicinchoninic acid (BCA)
184 protein assay (EuroClone). After normalization based on albumin concentration (assessed by
185 monodimensional gel electrophoresis), the same amount (10 μg) of proteins per sample was
186 separated by 2-DE (33). Briefly, plasma samples were diluted in 2.5% dithiothreitol (DTT) /5%
187 sodium dodecyl sulfate (SDS) and denatured at 95°C for 5 minutes. Then, they were diluted (250
188 μl) in UTC buffer (7M urea, 2M thiourea, 4% CHAPS) added with 0.04% ASB-14, 5% glycerol,
189 0.2% Tween-20, 100 mM DTT and 2% IPG buffer pH 4-7 (GE Healthcare). Samples were loaded
190 on 13 cm Immobiline™ DryStrip pH 4-7 (GE Healthcare) and isoelectric focusing was performed

191 with an Ettan™ IPGphor II system (Amersham Biosciences). Strips were equilibrated in 50 mM
192 Tris-HCl pH 8.8, 36% urea w/v, 2% SDS w/v, 67% glycerol v/v, bromophenol blue added with 1%
193 DTT (30 minutes incubation) and then with 2.5% IAA (30 minutes). Second dimension (based on
194 MW) was then performed on 12.5% polyacrylamide gels by SDS-PAGE. Gels were stained with
195 ProteinStain Fluo-R (SERVA) and acquired with a GelDoc-It™310 Imaging System (UVP), at four
196 different apertures (4.0, 5.6, 8.0 and 11).

197 Albumin proteoforms were identified, aligned and quantified using the ImageJ software. Briefly, a
198 linear background correction was applied (10 pixels rolling ball, sliding parabolooids) and all images
199 were aligned based on the main albumin protein spot (Registration plugin, alignment by line ROI).
200 Then, signals intensity was calculated for all albumin spots. The integrated density values of each
201 albumin proteoforms were normalized based on the sum of the intensities of all albumin spots per
202 sample. Results were expressed as mean±SEM in the two groups (Controls vs. Patients).

203

204 *Statistical analysis*

205 Data are expressed as mean±SD unless otherwise specified. Baseline data from patients and
206 controls were compared via t test or Mann-Whitney rank sum test, as appropriate. Different albumin
207 proteoforms were compared via two-tailed t-test, applying Benjamini-Hochberg correction for
208 multiple testing (FDR<0.05 as threshold). Pearson's correlation coefficient was employed to assess
209 the degree of linear relationship between two variables. Analysis was performed with SAS 9.4 (SAS
210 Institute Inc., USA). A P value <0.05 was considered statistically significant.

211

212 **Results**

213 Eighteen healthy controls and 18 septic patients were enrolled. Age (52 [47 – 60] vs. 58 [47 – 74]
214 years $p=0.32$), body mass index (23.4 [20.9 – 25.1] vs. 23.5 [20.8 – 26.0] kg/m^2 , $p=0.54$) and
215 gender (8 (44%) vs. 5 (28%) n (%)) of females, $p=0.49$) of healthy volunteers did not differ from
216 those of patients with sepsis. Septic patients had a SOFA score of 9 ± 2 points; eleven (61%) had
217 septic shock and were on vasopressors at the time of study. Infection sites were the lung in 9 (50%),
218 abdomen in 5 (28%), genitourinary tract in 3 (17%) and “other” in 1 (5%) case. Twelve patients
219 (67%) were mechanically ventilated, 3 (17%) were supported also by extracorporeal membrane
220 oxygenation and 2 (11%) were undergoing continuous renal replacement therapy. Overall
221 mortality of the studied population was 6 (33%). Patients received a median amount of 100 [0 –
222 300] ml of commercial 20% albumin (Albital, Kedrion, Italy) before the study time.

223 Baseline laboratory data and results of blood gas analysis performed on whole blood at 5%
224 of CO_2 are reported in **Table 1**. Of note, among non-carbonic buffers, hemoglobin and albumin
225 concentrations were significantly lower in septic patients ($p<0.01$), while phosphate concentrations
226 were similar in the two groups. Values of SID, Base Excess (BE) and HCO_3^- were significantly
227 lower in septic patients, while lactate concentration had a significantly higher value in this
228 population.

229

230 *Non-carbonic β of whole blood*

231 Tonometry of whole blood with 2, 5, 12 or 20% of CO_2 was performed to study *in-vitro* the capacity
232 of whole blood to resist to respiratory acid-base disorders. The experiments allowed to explore PCO_2
233 values between 13 and 138 mm Hg, with a resulting pH range of 6.83 to 7.81. As expected, the
234 increase in PCO_2 caused a decrease in pH and an increase in HCO_3^- (**Figure E1, Panel A and B**,
235 <https://doi.org/10.6084/m9.figshare.14398211.v1>). Consequently, there was a negative relationship
236 between HCO_3^- and pH. Individual pH and HCO_3^- values resulting from the equilibration process in

237 whole blood of healthy controls and septic patients are reported in **Figure 1A** and **1B**. Overall
238 HCO_3^-/pH curves for whole blood of the two study populations obtained by the polynomial
239 multilevel model are reported in **Figure E1, Panel C**. The resulting non-carbonic β/pH curves of
240 the populations, for the explored pH range, are two straight lines with equal slope and different
241 intercept ($p < 0.01$, see **Table E1**, <https://doi.org/10.6084/m9.figshare.14398250.v1>), resulting in
242 lower absolute β values in septic patients (**Figure E1, Panel D**).

243

244 *Non-carbonic β of isolated plasma*

245 Subsequently, to exclude red blood cells from the system, tonometry with 2, 5, 12 or 20% of CO_2
246 was performed on isolated plasma. This allowed to explore PCO_2 values between 16 and 130 mm
247 Hg, with a resulting pH range of 6.73 to 7.90. Individual experimental points of PCO_2 and the
248 resulting pH and HCO_3^- values for isolated plasma are reported in **Figure E2, Panels A and B**
249 (<https://doi.org/10.6084/m9.figshare.14398226.v1>). Absolute pH and HCO_3^- values of the study
250 populations resulting from the equilibration process in isolated plasma are reported in **Figure 2A**
251 and **2B**. Overall HCO_3^-/pH curves for isolated plasma of the two study populations obtained by the
252 polynomial multilevel model, are reported in **Figure E2, Panel C**. As for whole blood, the resulting
253 non-carbonic β/pH curves of the study populations, for the explored pH range, are two straight lines
254 with equal slope and different intercept ($p < 0.01$, see **Table E2**,
255 <https://doi.org/10.6084/m9.figshare.14398247.v1>), resulting in lower absolute non-carbonic β
256 values in septic patients (**Figure E2, Panel D**).

257

258 *Non-carbonic β of whole blood and isolated plasma at pH of 7.40*

259 To describe the capacity to resist to acid-base variations in normal conditions, absolute values of
260 non-carbonic β of both whole blood and isolated plasma were calculated at a pH value of 7.40.
261 Values of healthy volunteers were significantly higher than those of septic patients both for whole

262 blood (31.6 ± 2.1 vs. 22.0 ± 1.9 mmol/L, $p < 0.01$) and isolated plasma (3.7 ± 0.8 vs. 0.5 ± 1.0 mmol/L,
263 $p < 0.01$), as shown in **Figure 3**. Of note, for both patients and controls, isolated plasma had
264 significantly lower values of non-carbonic β as compared to whole blood ($p < 0.01$, for both).

265

266 ***Buffering mechanisms***

267 *a. Whole blood*

268 The mechanisms underlying the buffering capacity of whole blood were then investigated and
269 changes in sodium, chloride and SID consequent to the applied PCO_2 were assessed. When passing
270 from the lowest (around 20 mm Hg) to the highest PCO_2 (around 120 mm Hg), a significant increase
271 in sodium concentration (5 ± 1 mmol/L vs. 4 ± 1 mmol/L, $p < 0.01$, in healthy volunteers and septic
272 patients, respectively) and reduction in chloride concentration (7 ± 1 mmol/L and 5 ± 1 mmol/L,
273 $p < 0.01$, in healthy volunteers and septic patients, respectively) was observed (**Figure E3, Panel A**
274 **and B**, <https://doi.org/10.6084/m9.figshare.14398244.v1>). On the contrary, no significant variations in
275 potassium were observed. Changes in sodium and chloride in the two populations, according to the
276 pH changes resulting from CO_2 -tonometry are provided in **Figure E4**
277 (<https://doi.org/10.6084/m9.figshare.14398238.v2>). As a result, a significant increase in SID
278 (13.5 ± 1.2 mEq/L and 9.8 ± 1.4 mEq/L, $p < 0.01$, in healthy volunteers and septic patients,
279 respectively) was observed with the maximum PCO_2 variation (**Figure 4A and 4B**).

280 The contribution of electrolyte shifts to total non-carbonic β of blood (non-carbonic β_{SID}) was
281 then computed. Overall SID/pH curves for the two study groups are reported in **Figure E3, Panel**
282 **C**. The resulting function describing non-carbonic β_{SID} in the explored pH range was a horizontal
283 line (**Figure E3, Panel D**). According to this model (**Table E3**,
284 <https://doi.org/10.6084/m9.figshare.14398223.v1>), β_{SID} of whole blood is therefore independent
285 from pH values. Furthermore, significantly lower values of β_{SID} were observed in septic patients as
286 compared to controls (16.8 ± 1.9 vs. 24.4 ± 1.9 mmol/L, $p < 0.01$, **Figure 5**). A strong correlation

287 (r=0.94, p<0.01) between hemoglobin concentration and β_{SID} was found when pooling data from
288 both groups (**Figure 6**).

289 *b. Isolated plasma*

290 A possible correlation between albumin concentration and non-carbonic β of isolated plasma was
291 investigated to understand the mechanisms underlying the buffering capacity of isolated plasma.

292 A strong correlation (r=0.93, p<0.01) was observed when pooling data from both groups (**Figure**
293 **E5**, <https://doi.org/10.6084/m9.figshare.14720898.v1>). In addition, the representative values
294 obtained at pH = 7.40 of non-carbonic β of isolated plasma normalized for albumin concentration
295 (β_{NORM}) were compared in order to assess possible differences of albumin buffering capacity. Septic
296 patients had significantly lower values of β_{NORM} (0.01 [-0.01 – 0.04] vs. 0.08 [0.06 – 0.09] mmol/g, p
297 <0.01) as compared to controls (**Figure 7**). In addition, a different amount of specific albumin
298 proteoforms was observed by two-dimensional electrophoretic separation of plasma samples
299 (**Figure 8A**). In particular, amongst the nine detected albumin proteoforms, in septic patients a
300 significant increase (FDR<0.05) in the amount of the acidic ones was observed (spots 7 and 9),
301 accompanied by a downward trend of the alkaline ones (spots 1, 2 and 3) (**Figure 8B**).

302

303 **Discussion**

304 In the present study, respiratory acid-base derangements were induced *in-vitro*. We simulated
305 hypoventilation/hypercapnia by equilibrating our samples with gases containing high CO₂
306 concentrations. Moreover, hyperventilation/hypocapnia was simulated using gases containing a low
307 CO₂ concentration. This allowed to measure the *in-vitro* non-carbonic β , *i.e.* the capacity of
308 blood/plasma to limit pH changes secondary to acute PCO₂ variations, in septic patients and healthy
309 volunteers. Our main finding is that septic patients' capacity to buffer respiratory acid-base
310 disorders is markedly reduced (approximately by 30%) as compared to healthy volunteers. This, of
311 course, exposes this category of patients to more pronounced pH variations for any given
312 respiratory and/or metabolic acid-base derangement. The reduced non-carbonic β of septic patients
313 is due to two major factors. First, and more importantly, this category of patients has lower
314 concentrations of non-carbonic buffers. Indeed, both hemoglobin and albumin concentrations were
315 significantly lower (**Table 1**). Second, it appears that septic patients' albumin has a reduced
316 buffering capacity. Indeed, when normalizing the non-carbonic β of isolated plasma by the
317 measured albumin concentration, we found significantly lower buffering capacity for every gram of
318 plasma albumin (**Figure 7**). This finding suggests that the molar buffering capacity of the protein
319 macromolecule might be altered by critical illness and/or by the administration of exogenous
320 albumin. The difference observed in albumin proteoforms (Figure 8) supports this finding. In other
321 words, these results suggest that the protein buffering system of septic patients might have different
322 acid dissociation constants. In addition, it has been demonstrated that commercial albumin,
323 frequently administered to our patients, has an altered red-ox state (41). However, how this red-ox
324 state alteration affects albumin buffering capacity and its acid dissociation constant needs to be
325 determined in further studies, properly designed to address this question.

326

327 In addition, the present study shed light on the physiologic and pathophysiologic
328 mechanisms of buffering during acute respiratory acid-base derangements. In line with previous
329 studies performed in the setting of metabolic acid-base disorders (34, 35), our data show, overall,
330 that whole blood has a significantly higher buffering capacity as compared to isolated plasma
331 (**Figure 3**). To understand the underlying mechanisms, we partitioned and quantified the two
332 components of non-carbonic buffer power, *i.e.* i) changes in electrolytes induced by PCO_2
333 variations, resulting in variations in SID and ii) variations in the dissociation/association of plasma
334 proteins.

335 We observed that electrolytes vary remarkably, when PCO_2 is changed acutely in whole
336 blood. Indeed, when the PCO_2 of whole blood is increased through tonometry, chloride decreases
337 significantly (**Figure E3, Panel B**). Moreover, a concomitant significant increase in sodium
338 concentration was observed. Interestingly, similar results were reported by Giebisch in *in-vivo*
339 experiments performed in dogs (8). When analyzing intracellular fluid, the authors did not find a
340 reduced sodium concentration, suggesting that the increase in sodium observed during respiratory
341 acidosis was not caused by a shift from the red blood cell. This difference between our results and
342 the finding of Giebisch and colleagues could be explained by known differences between canine
343 and human red blood cell physiology (36). Another factor potentially at play is the salt-type
344 binding/unbinding of electrolytes to large proteins, which appears to be influenced by PCO_2 and pH
345 (27, 37-39).

346 The result of the observed electrolyte shifts secondary to a primary increase in PCO_2 was an
347 increase in SID up to 15 mmol/L (**Figure 4**). As an increase in SID favors an increase in HCO_3^- ,
348 and shifts the system towards alkalosis, it is clear that this mechanism of interdependence between
349 PCO_2 and SID during respiratory acid-base disorders limits the resulting pH changes of whole blood
350 (19). Of note, in the present study hemoglobin was always completely saturated with oxygen. The
351 contribution of the Haldane effect, with the related chloride shift due to the transition of hemoglobin

352 from the deoxygenated tense (T-state) to the oxygenated relaxed (R-state), could thus be excluded
353 as contributing factor to the observed electrolyte shifts (40, 41).

354 We therefore quantified the contribution of SID variations to the non-carbonic β and called
355 this term β_{SID} . The aim of this analysis was to quantify the changes in HCO_3^- secondary to CO_2
356 variations determined by electrolyte shifts. It is worth underlining that the SID changes observed in
357 whole blood samples were secondary to electrolyte shifts from and to the red blood cells, as no
358 electrolytes were added or removed from the sample. Moreover, it is important to state that the β_{SID}
359 concept used in the present study differs significantly from other studies, in which PCO_2 was kept
360 constant, SID was changed through the addition of strong acids or bases, and the resulting pH
361 variation was assessed (42).

362

363 In both healthy volunteers and septic patients, we found that the electrolyte shift and
364 therefore β_{SID} is undoubtedly the most important buffering mechanism of blood, accounting for
365 approximately 80% of the total non-carbonic buffering capacity (**Figure 5**).

366 Interestingly, the value of β_{SID} was found to be, in the explored pH range, independent from
367 pH (**Figure E3, Panel D**), *i.e.* in our model the “hemoglobin-red blood cell” buffering system does
368 not seem to behave as a weak acid, but seems to have a fixed, pH-independent buffering effect.
369 Finally, we were able to demonstrate that the interindividual differences in PCO_2 -induced SID
370 variations (**Figure 4**) and therefore the differences in β_{SID} were strongly correlated with hemoglobin
371 concentration, a reasonable proxy of red blood cell intracellular volume (**Figure 6**).

372 When studying isolated plasma, we were able to exclude the buffering function of the
373 “hemoglobin-red blood cell” system, and therefore focused our attention on a second physiologic
374 mechanism, *i.e.* the variations in dissociation/association of plasma proteins (15, 16). Also in the
375 experiments performed on isolated plasma, we found significant differences in the buffering
376 capacities of healthy volunteers and septic patients (**Figure 3**). This finding is certainly explained,

377 at least in part, by a lower albumin concentration in septic patients (**Table 1**). Nevertheless, also
378 when normalizing the non-carbonic β for measured albumin (the major non-carbonic buffer of
379 plasma) we found lower values in patients. This finding suggests that the molar buffering capacity
380 of the protein macromolecule might be altered by critical illness and/or by the administration of
381 exogenous albumin. The difference observed in albumin proteoforms (**Figure 8**) supports this
382 finding. In other words, these results suggest that the protein buffering system of septic patients
383 might have different acid dissociation constants. In addition, it has been demonstrated that
384 commercial albumin, frequently administered to our patients, has an altered red-ox state (43).
385 However, how this red-ox state alteration affects albumin buffering capacity and its acid
386 dissociation constant needs to be determined in further studies, properly designed to address this
387 question.

388

389 **Clinical implications**

390 Our study suggests that septic patients, due to lower buffer concentration and, possibly, an altered
391 buffering function of albumin, are more exposed to acute acid-base derangements. In line with
392 previous studies (44, 45), we clearly observed that the “hemoglobin-red blood cell” system is by far
393 the most important buffering mechanism. It is thus clear that the red blood cell transfusion strategy
394 (46, 47) will have a significant impact on the ability of blood to resist to acid-base perturbations,
395 with a more liberal strategy being associated with higher non-carbonic buffer power and a more
396 restrictive strategy with a lower capacity to resist to respiratory acid-base derangements. In
397 addition, the *in-vitro* carbon dioxide titration curve that we performed clearly underlines the
398 importance of tailoring nomograms to the specific clinical condition. Indeed, rules frequently
399 applied in critical care to predict changes in HCO_3^- following an acute hypercapnia (48) or
400 hypocapnia (49) are derived from healthy volunteers or from healthy surgical patients, *i.e.* not from
401 critically ill patients. In addition, the studies that derived these rules hardly discussed the buffering

402 role of the “hemoglobin-red blood cell” system, which, as previously observed (44, 45) and
403 confirmed by our data, is by far the major non-carbonic buffer. Finally, it is important to mention
404 that non-carbonic buffer power is employed in all equations used to calculate base excess (50-52).
405 Many equations estimate the non-carbonic buffer power according to the hemoglobin concentration,
406 other equations, such as the “Van Slyke equation” introduced by Siggaard-Andersen and suggested
407 by the Clinical and Laboratory Standards Institute (CLSI) (31) assume a constant value of 16.2
408 mmol/L for the extracellular fluid (50). This value was derived from *in-vivo* experiments performed
409 in 8 healthy subjects undergoing either voluntary hyperventilation or inhalation of CO₂ (53). The
410 author thus derived the following equation: $\beta = 2.3 \cdot \text{ctHb (Ecf)} - 7.7$ mmol/L, which yields a value
411 of -16.2 mmol/L for a blood hemoglobin concentration of 16 g/dL and a total protein concentration
412 of 7 g/dL (53, 54). While changes in the non-carbonic buffer power have a small effect in the
413 computation of Base Excess (50), our study describes the variability of whole blood non-carbonic
414 buffer power in septic patients (range between 20 and 28 mmol/L), caused both by the variability of
415 hemoglobin and albumin concentration, and by different acid-base characteristics (β_{NORM}) of
416 albumin. These findings hence underline the importance of using personalized values in order to
417 compute accurate base excess values.

418

419 **Limitations**

420 We need to mention some limitation of our study. The *in-vitro* nature of the study, while allowing
421 to exclude confounding factors, such as intravenous fluid therapy (55-58), did exclude the
422 interaction with the interstitium which is certainly clinically relevant. Brackett et al (48) suggest
423 that the *in-vivo* non-carbonic β is lower than the equivalent *in-vitro* determination due to a higher
424 volume of distribution (59). This aspect, which needs to be clarified in future clinical studies, might
425 be exacerbated in critically ill patients, frequently characterized by an expanded extracellular
426 volume. Another limitation of our study relies in the fact that we analyzed whole blood, *i.e.* the

427 “plasma-red blood cell system”. Our data therefore do not allow to draw conclusions on the
428 “buffering” role of free hemoglobin. Moreover, we have no information on the intracellular effects
429 of CO₂- tonometry. Finally, our data suggest that plasma proteins of septic patients might have a
430 lower acid dissociation constant. However, in our experimental design we explored only 4 different
431 partial pressures of CO₂ which did not allow us to determine experimentally the dissociation
432 constant (27). Future studies are warranted to determine the acid dissociation constant of septic
433 patients’ plasma proteins.

434

435 **Conclusions**

436 Septic patients, as compared to healthy volunteers, have a reduced non-carbonic β , which exposes
437 this category of patients to more pronounced pH shifts for any given respiratory acid-base
438 derangement. Moreover, the reduced non-carbonic β likely exposes these patients also to greater pH
439 shifts during metabolic acid-base derangements. The “hemoglobin-red blood cell” system is by far
440 the most important buffering mechanism and seems to be pH-independent, *i.e.* it does not behave as
441 a classic buffer in the explored pH range. Indeed, this system limits pH changes through electrolyte
442 shifts determining variations in SID, proportional to the variation in PCO₂. This finding, besides
443 underlining the interdependence of PCO₂ and SID, suggests that the pathophysiology of acid-base
444 equilibrium is far from being fully understood.

445

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451 Maggiore Policlinico, Milan, for their administrative and logistical support.

452

453 **Availability of data and materials**

454 The complete dataset is available at the following link:

455 <https://doi.org/10.6084/m9.figshare.14709609.v2>

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- 615
- 616
- 617

618 FIGURE AND TABLE LEGEND

619

620 Figure 1. pH to bicarbonate relationship in whole blood.

621 Experimental points of pH and HCO_3^- concentration obtained through equilibration of whole blood
622 at different PCO_2 values in healthy controls (Panel **A**) and septic patients (Panel **B**). Each
623 subject/patient is identified by a different symbol.

624

625 Figure 2. pH to bicarbonate relationship in isolated plasma

626 Experimental points of pH and HCO_3^- concentration obtained through equilibration of isolated
627 plasma at different PCO_2 values in healthy controls (Panel **A**) and septic patients (Panel **B**). Each
628 subject/patient is identified by a different symbol.

629

630 Figure 3. Non-carbonic β at pH 7.40.

631 Representative values at $\text{pH} = 7.40$ for non-carbonic buffer power (β) in healthy controls and septic
632 patients for whole blood (left side of the graph) and isolated plasma (right side of the graph). Dots
633 represent 5th and 95th percentiles.

634

635 Figure 4. PCO_2 to SID relationship in whole blood

636 Experimental points of PCO_2 and Strong Ion Difference (SID) obtained through equilibration of
637 whole blood at different PCO_2 values in healthy controls (Panel **A**) and septic patients (Panel **B**).
638 Each subject/patient is identified by a different symbol.

639

640 Figure 5. Non-carbonic β due to SID variations in whole blood

641 Values of the buffer component due to SID variation (β_{SID}) in whole blood of healthy controls and
642 septic patients. These values are independent of the applied pH, as β_{SID} did not change with pH in the
643 explored PCO_2 range. Dots represent 5th and 95th percentiles.

644

645 Figure 6. Hemoglobin to β_{SID} variation relationship

646 Relationship between hemoglobin and β_{SID} in the whole study population. Black circles represent
647 data from control subjects, while white circles represent data from septic patients. A strong
648 correlation was found for the overall population. A similar finding was observed, when analyzing
649 Patients ($r = 0.74$, $p < 0.01$) and Controls ($r = 0.61$, $p < 0.01$) separately.

650

651 Figure 7. Normalized non-carbonic β of plasma at pH = 7.40

652 Representative values of non-carbonic β of isolated plasma at pH = 7.40 normalized for albumin
653 concentrations (β_{NORM}). Dots represent 5th and 95th percentiles.

654

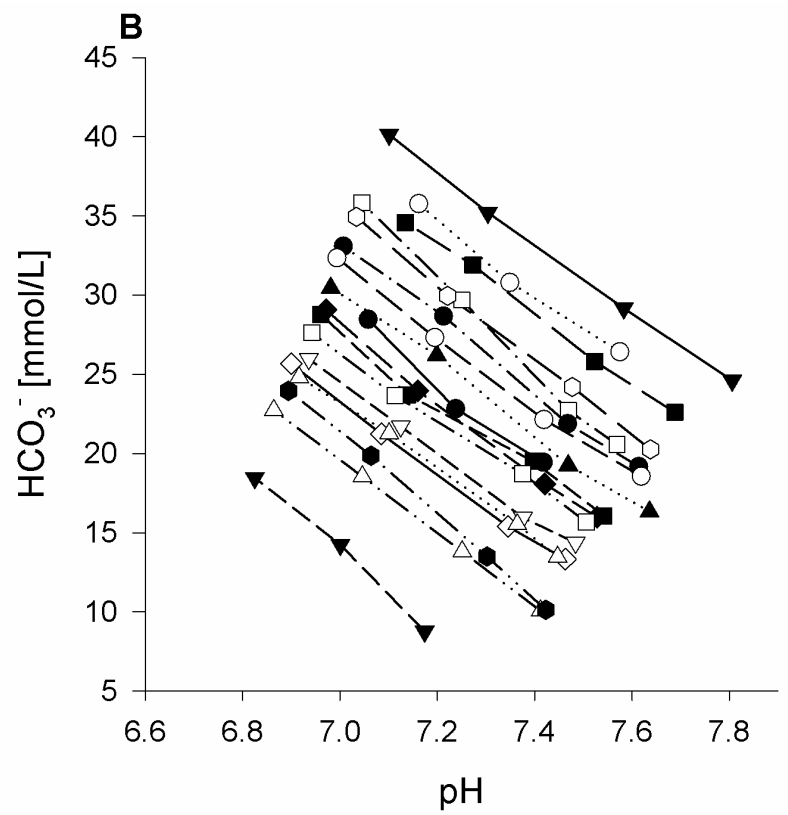
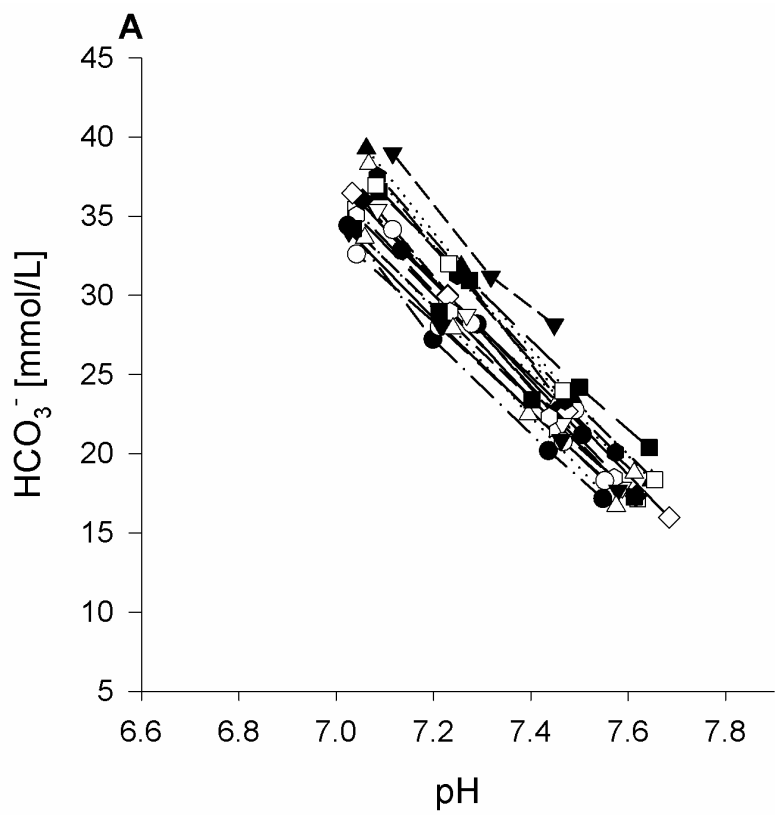
655 Figure 8. Albumin proteoforms.

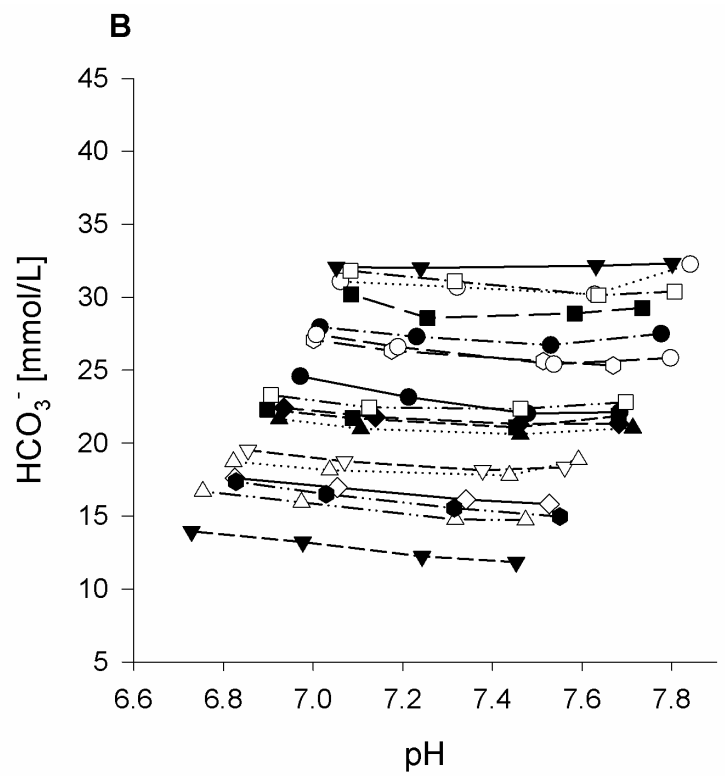
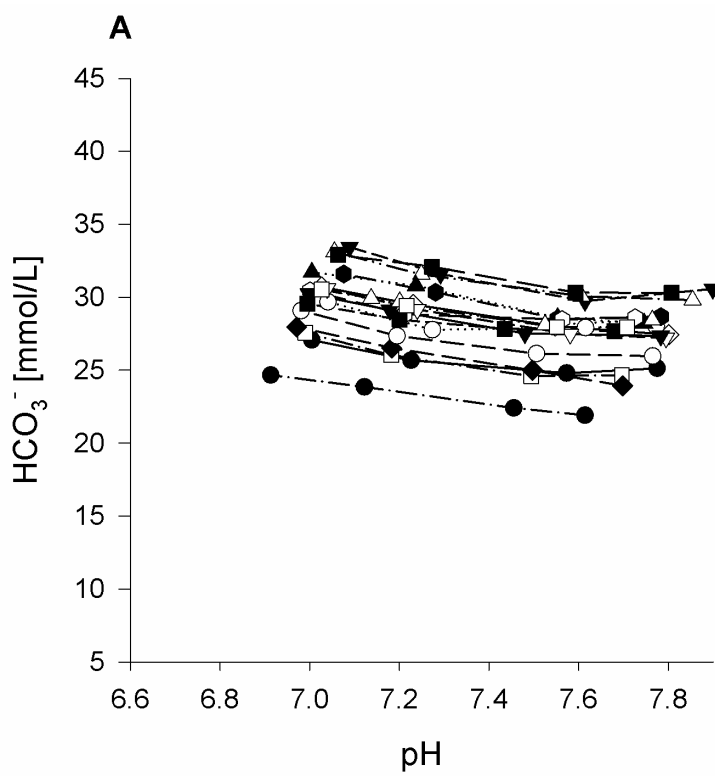
656 **A)** Representative map of plasma proteins after two-dimensional electrophoresis (2-DE). Proteins
657 were separated horizontally by their isoelectric point (plus end: acidic; minus end: alkaline) and
658 then vertically by their molecular weight (MW). Lane 1: protein marker. Lane 2: loading control
659 (10 μg). Inset image: magnification of albumin proteoforms, identified by nine adjacent spots. **B)**
660 Quantification of albumin proteoforms after 2-DE. *FDR < 0.05.

661

662 Table 1. Baseline laboratory values and blood gases and electrolytes obtained at 5% of CO₂.

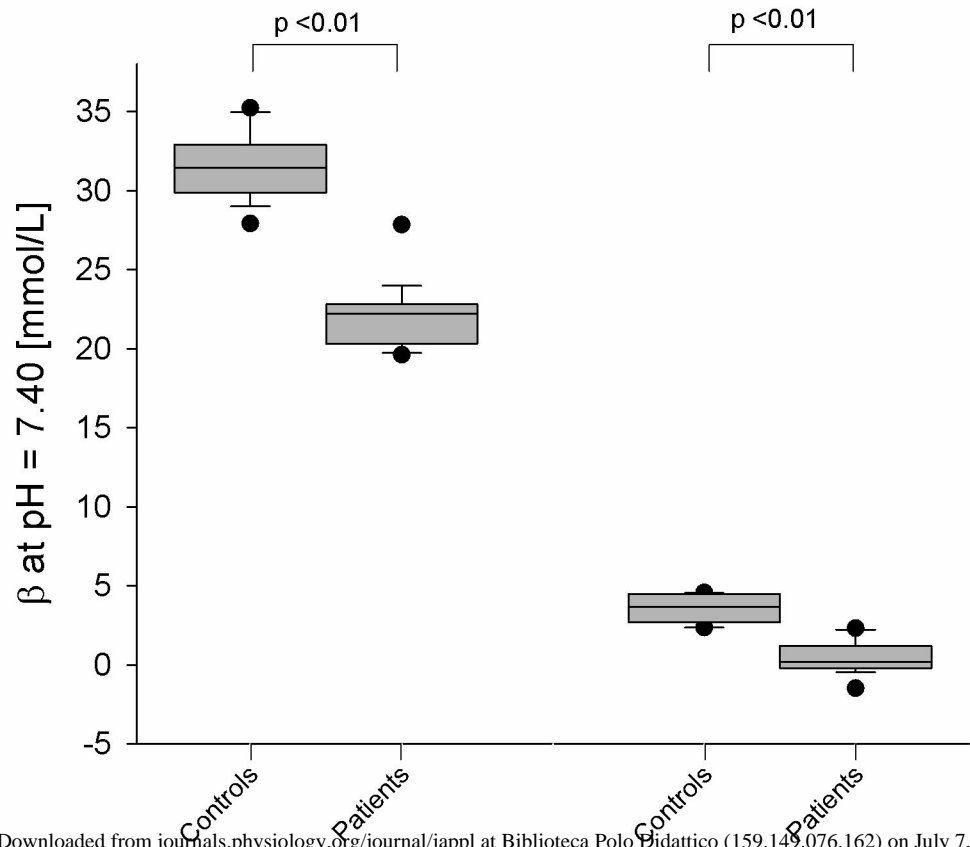
663 Baseline laboratory data for albumin, total proteins, phosphates and hemoglobin concentrations, and
664 results of gas analysis performed on whole blood at 5% of CO₂. P values refer to t-test or Mann-
665 Whitney rank sum test, as appropriate.

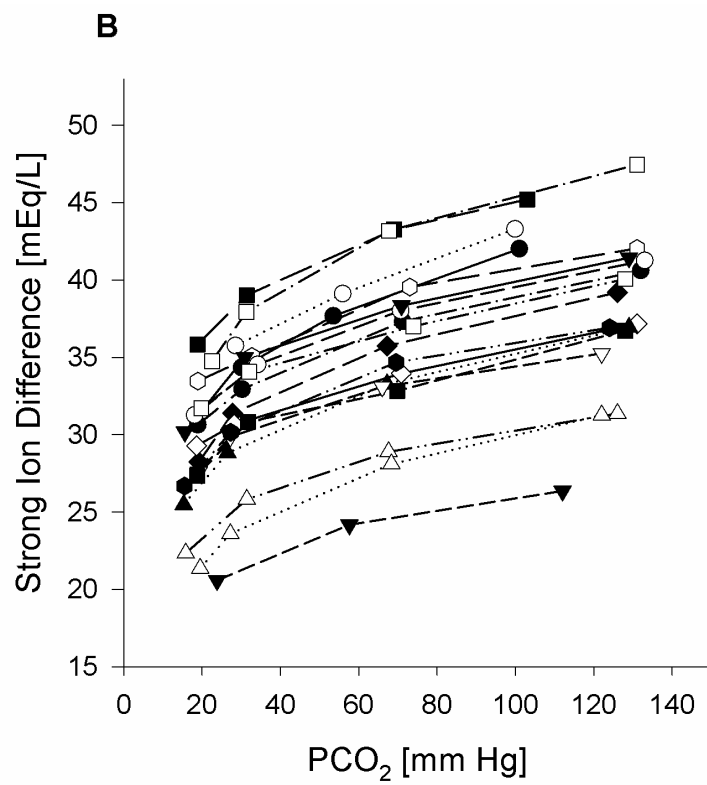
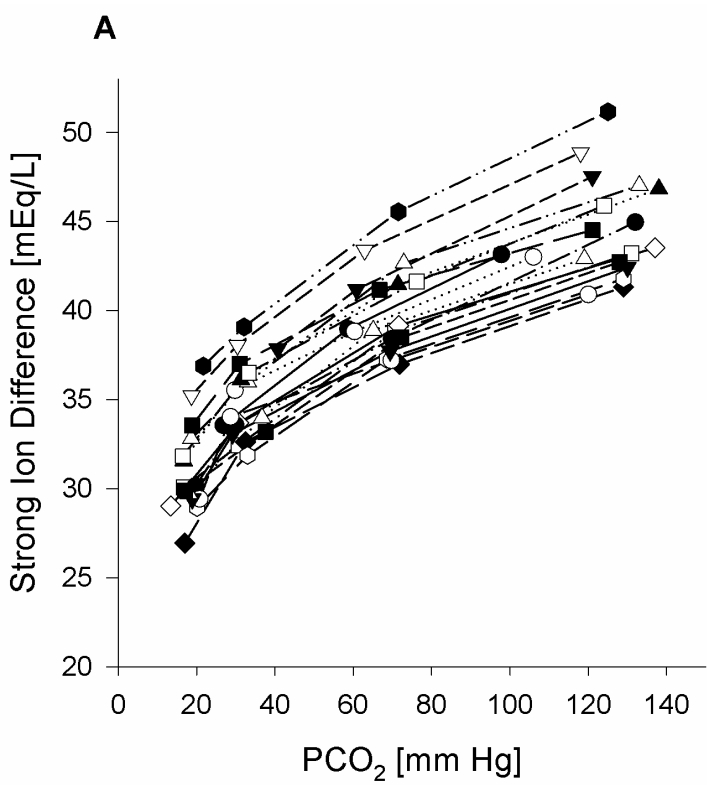


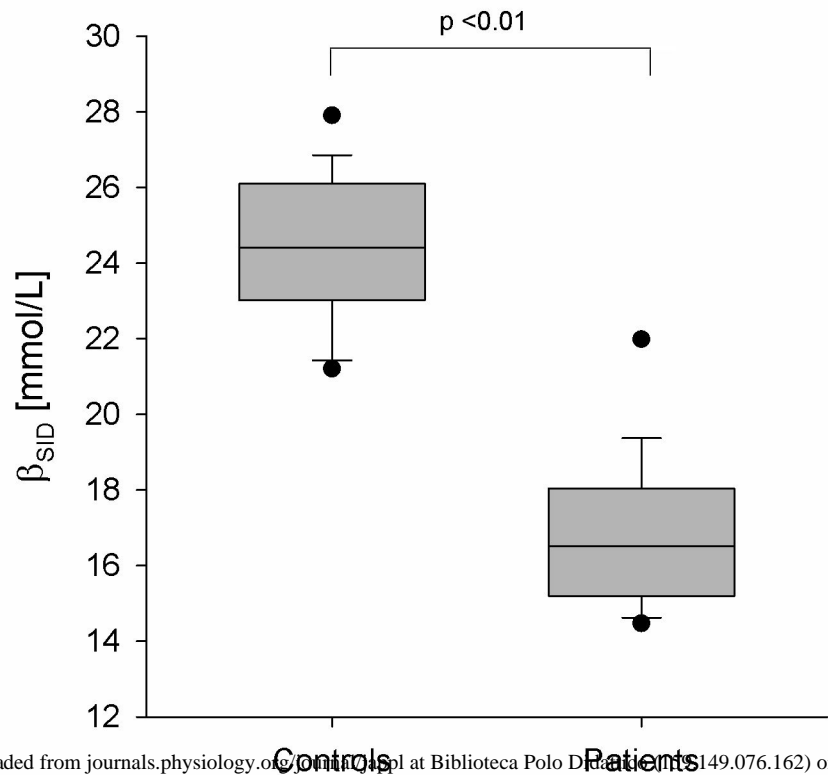


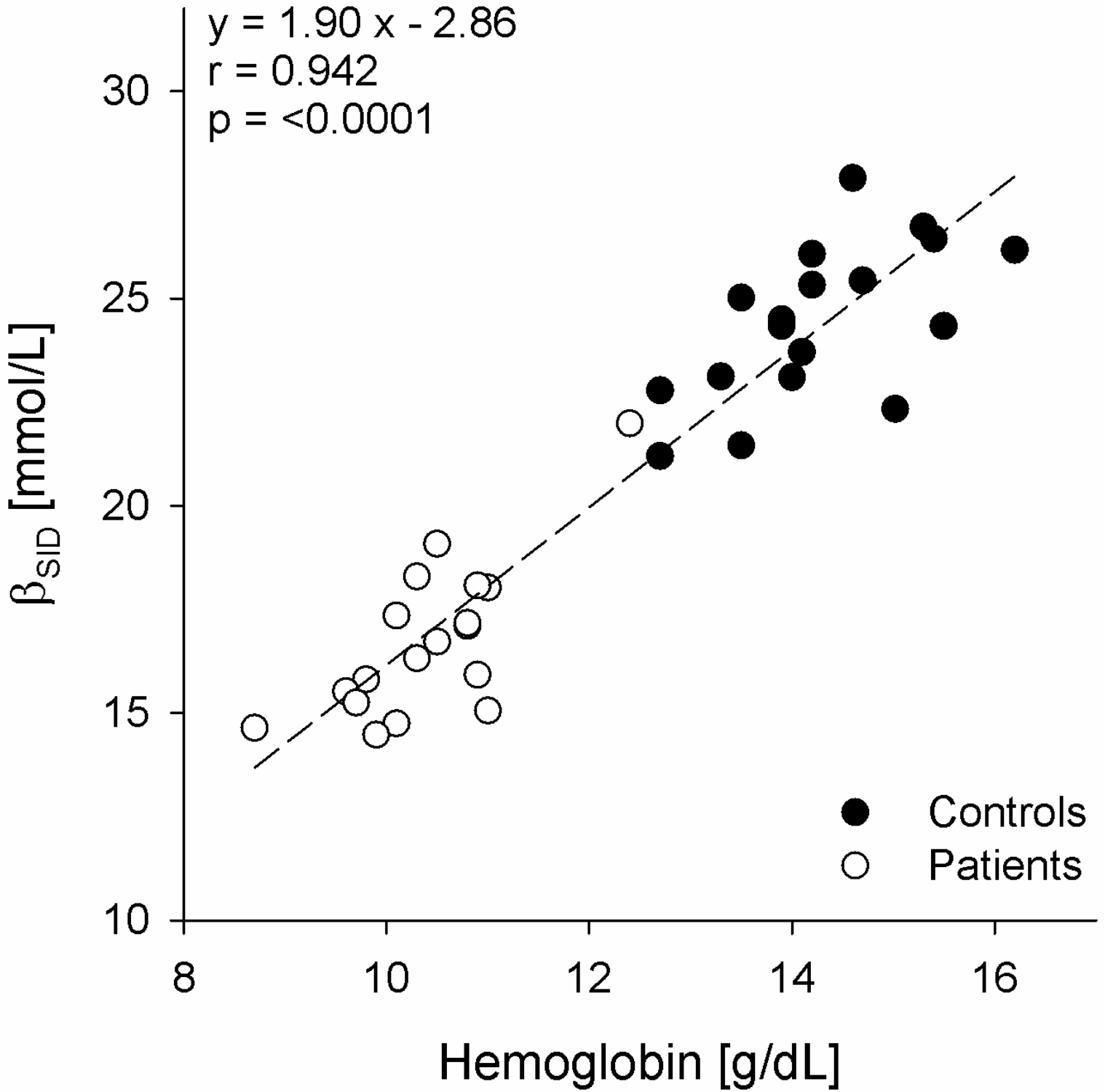
BLOOD

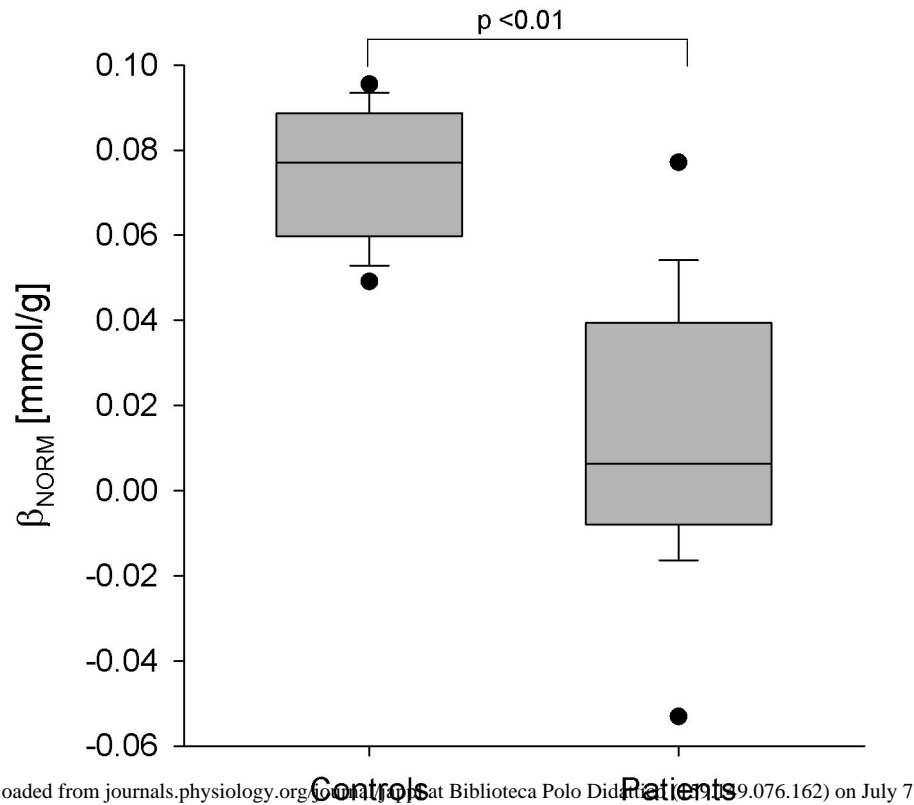
PLASMA

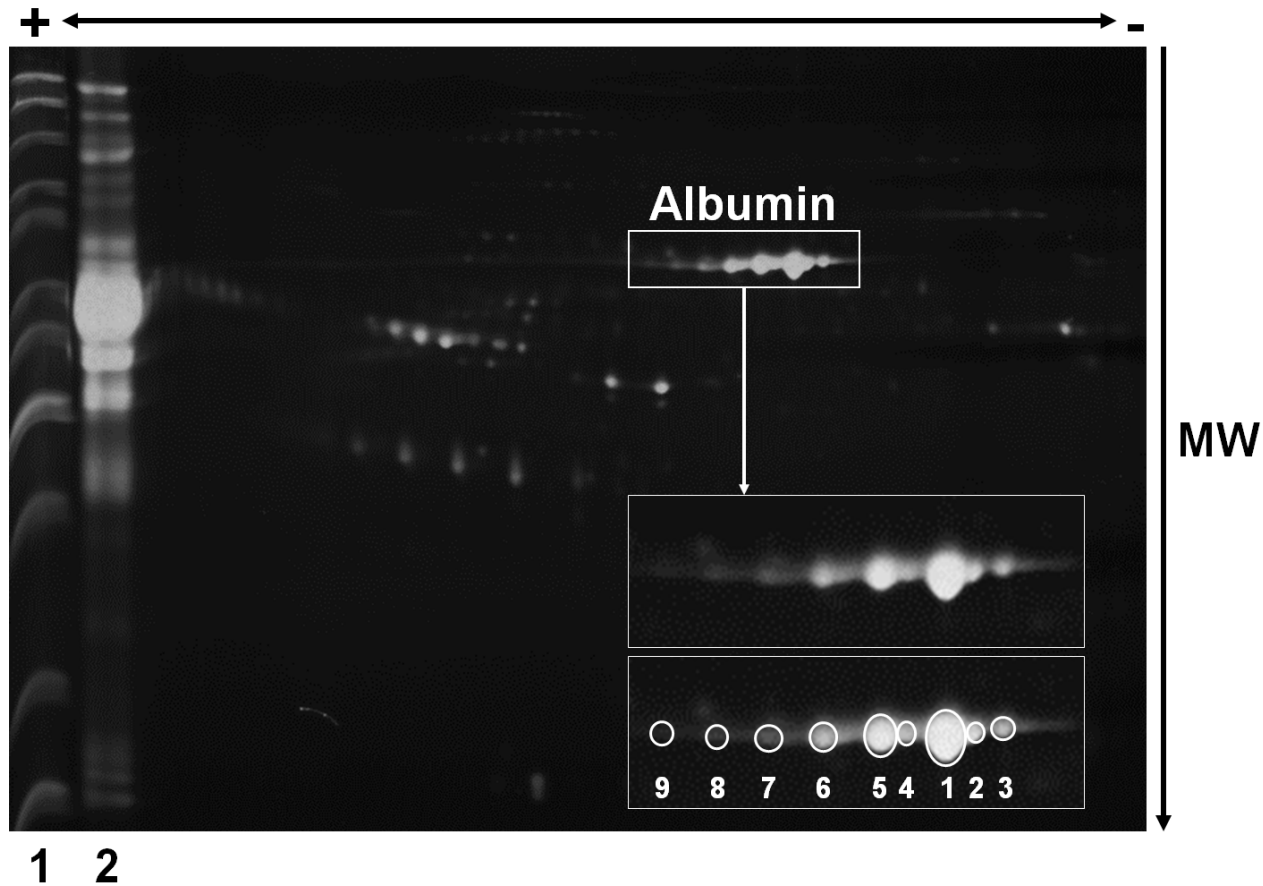










A**B**

Albumin proteoforms

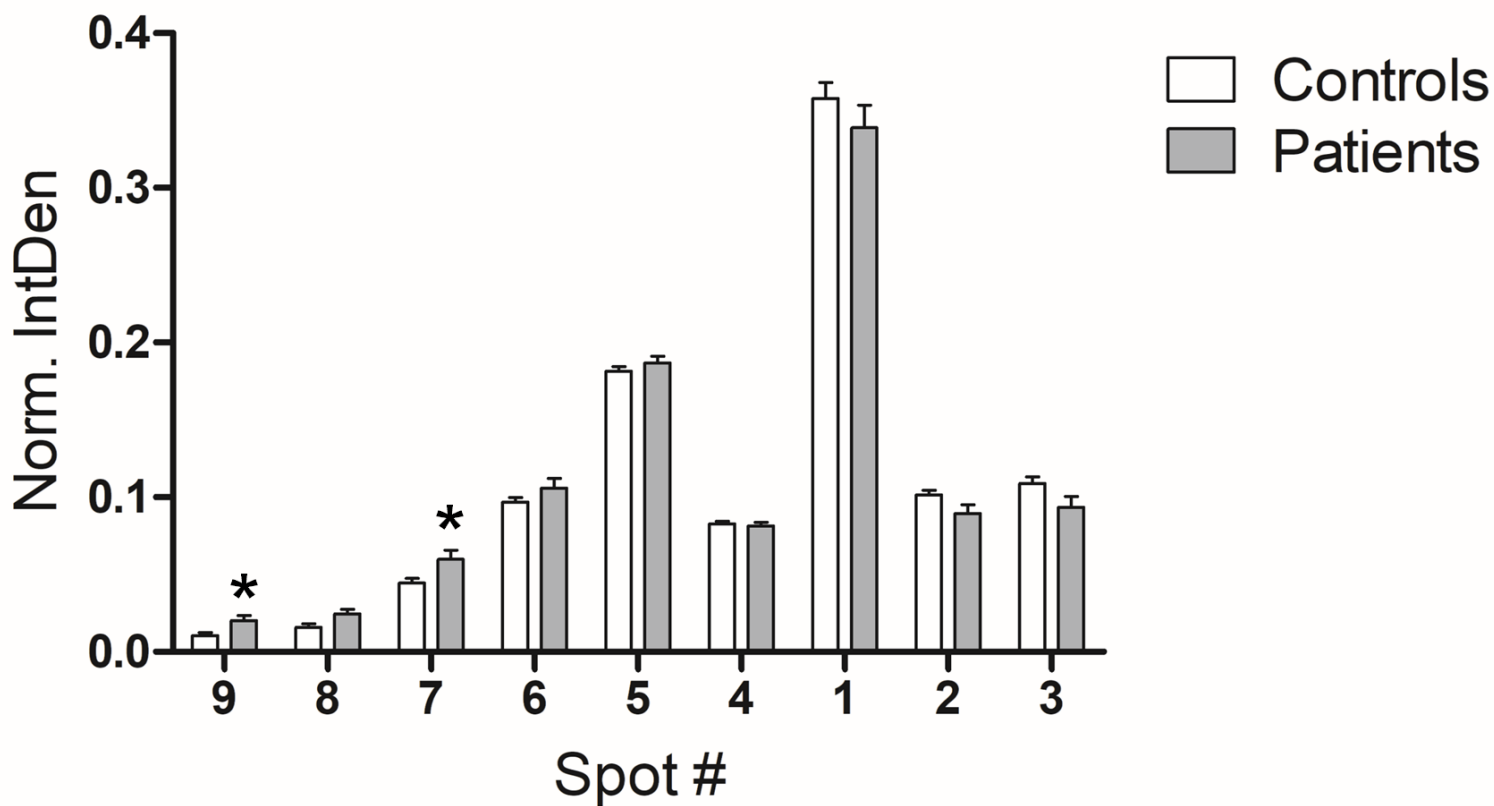


Table 1

	Controls (n=18)	Patients (n=18)	P
Albumin [g/dL]	4.7 [4.6 – 4.9]	3.0 [2.8 – 3.2]	<0.01
Hemoglobin [g/dL]	14.3 ± 1.0	10.4 ± 0.8	<0.01
Hematocrit [%]	41 [40 – 44]	30 [29 – 32]	<0.01
Phosphate [mg/dL]	3.4 [2.9 – 3.5]	4.4 [2.8 – 5.3]	0.12
pH	7.463 [7.446 – 7.477]	7.418 [7.359 – 7.471]	0.11
PCO ₂ [mm Hg]	31.2 [30.0 – 33.2]	30.2 [27.3 – 31.5]	0.05
HCO ₃ ⁻ [mmol/L]	20.9 [19.9 – 21.7]	17.9 [14.3 – 21.4]	0.03
Na ⁺ [mmol/L]	139 [137 - 140]	139 [135 - 144]	0.78
K ⁺ [mmol/L]	4.3 ± 0.4	4.3 ± 0.6	0.65
Ionized Ca ²⁺ [mmol/L]	1.16 [1.13 – 1.20]	1.08 [1.06 – 1.14]	<0.01
Total Calcium [mg/dL]	9.5 ± 0.3	7.8 ± 0.2	<0.01
Magnesium [mg/dL]	2.1 [2.0 – 2.2]	2.0 [1.9 – 2.3]	0.40
Cl ⁻ [mEq/L]	108 [108 – 110]	111 [107 – 113]	0.31
Lactate ⁻ [mmol/L]	1.7 [1.1 – 2.1]	2.0 [1.7 – 5.2]	0.01
SID [mEq/L]	34.0 [33.2 – 36.6]	32.2 [29.6 – 35.0]	0.04
BE [mmol/L]	-1.2 [-2.0 – -0.1]	-4.8 [-9.2 – -0.5]	0.02