

1 **Surgical repair of an unicortical condylar fracture in a Thoroughbred racehorse**
2 **using a bioabsorbable screw**

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27 author.

28 **Abstract**

29 Surgical repair of unicortical fractures of the distal condyles of the third
30 metacarpal/metatarsal bones (MCIII/MTIII) has been described. In the present case, a
31 bioabsorbable screw was used to stabilize a unicortical fracture in the palmar aspect
32 of the medial condyle of MCIII in a National Hunt Thoroughbred racehorse. The
33 clinical, radiographic and magnetic resonance (MRI) findings before and after surgery
34 were recorded. Eighteen weeks after surgery, the lameness had resolved and the bone
35 surrounding the fracture had recovered its normal architecture. One year after surgery,
36 the horse was in training, showed no recurrence of the primary lesion and was
37 considered a “racing prospect” by the trainer.

38 The use of a bioabsorbable screw in this case was associated with a successful
39 outcome and is worthy of further investigation.

40 **Keywords:** horse, bioabsorbable screw, condylar fracture, MRI, osteointegration.

41 **Introduction**

42 Unicortical condylar fractures of the distal condyles of the third metacarpal/metatarsal
43 bone (MCIII/MTIII), an early stage of the more commonly recognized
44 complete/incomplete (bicortical) condylar fracture, are common injuries in
45 racehorses. In literature they are defined as short fractures, fissures, or incomplete
46 fractures and often originate to the palmar/plantar aspect of the bone in the area where
47 the sesamoid bones articulate with the condyle [1–3]. In the literature, the
48 pathogenesis of these fractures involves progressive, fatigue related disease of the
49 mineralized cartilage and subchondral bone and often originates in the palmar/plantar

50 aspect of the medial or lateral condylar groove [4]. Surgical treatment is generally
51 recommended in order to stabilize the fracture and thereby prevent its further
52 propagation and encourage healing. Brown *et al.* [5] suggested that the placement of a
53 single lag screw in unicortical condylar fractures may be useful for reducing the
54 recovery period. While complications associated with the use of metal screws in this
55 location are uncommon, it is known the risk of osteolysis around the implant, which
56 although not always clinically relevant, can determine unwanted changes in the
57 material properties of the bone [6]. Bioabsorbable implants, including bone screws,
58 are increasingly used in human orthopaedic surgery [7–9]. These implants can be
59 classified into several categories depending on their composition. Some are made
60 from synthetic polymers, such as polyglycolic or poly L-lactide acid (PLLA), poly-d-
61 lactate, or polyethylene. Others are composed of ceramics, while others are made of a
62 composite of bioceramic and polymers. The use of bioabsorbable implants in the
63 horse was first reported by Field *et al.* in 1993, who evaluated the mechanical
64 properties of bioabsorbable screws in bones from horse cadavers. They concluded that
65 bioabsorbable screws used to stabilise a fissure created from the sagittal ridge to
66 middle-diaphysis of the distal third metacarpal/metatarsal bone were inferior to those
67 made of stainless steel in achieving stability of the repair construct [10]. Wall *et al.*
68 [11] reported successfully using bioabsorbable screw to bridge the physis of long
69 bones in foals as a means of correcting angular limb deformities. Pyles *et al.* [12]
70 investigated the efficacy of using a bioabsorbable screw to repair an induced fracture
71 in the proximal sesamoid bone, while Mageed *et al.* [13] reported using bioabsorbable
72 screws to treat a splint bone fracture. All the aforementioned studies used implants
73 made of polymers. This case report describes the successful management of a
74 unicortical fracture in the distal condyle of MCIII using a composite bioabsorbable

75 screw. This implant has been shown to retain high strength during fracture healing, is
76 absorbed, has osteoconductive properties and binds well to surrounding bone matrix
77 [14].

78 **1. Case Report**

79 **1.1 Case history**

80 A 2-year-old National Hunt Thoroughbred racehorse (520 kg bodyweight) was
81 admitted for investigation of right forelimb lameness that developed acutely after the
82 morning workout.

83 **2.2 Clinical findings**

84 The horse was grade 3 lame (AAEP scale 1-5)[15] on the right forelimb. It showed
85 pain when the right fore fetlock joint was flexed although the joint was not swollen.
86 No intra-articular medications of the injured fetlock joint were performed prior to
87 diagnosis.

88 **2.3 Diagnosis**

89 A radiographic examination of the right fore fetlock was performed. A radiolucent
90 line, compatible with a unicortical condylar fracture of the palmar aspect of the
91 medial condyle of MCIII (Fig 1A) was identified on the dorsodistal-palmaro proximal
92 oblique (flexed dorsopalmar) projection. In order to confirm the diagnosis, a standing
93 magnetic resonance imaging (MRI) (Hallmarq¹, Tesla 0.27) examination was
94 performed. The horse was sedated with detomidine (0.02 mg/kg i.v.) and butorphanol
95 (0.06 mg/kg i.v.) and MRI of the metacarpophalangeal joint was performed including
96 the following sequences: palmar-sagittal aspect using gradient T1, T1 HR (High
97 Resolution), T2* (T2-star), FSE (Fast Spin Echo), T2 FAT-SAT (Fat Saturation); in
98 sagittal aspect with T1 FAT-SAT and in dorsal aspect using T1, T1 HR and FAT-
99 SAT. The MRI images confirmed the presence of a 1cm fissure in the sagittal plan

100 located in the palmar cortex of the condylar groove of the medial condyle. The fissure
101 was associated with bone resorption, fluid signal around the fissure and sclerosis of
102 the surrounding bone (Fig 1B-F).

103 Surgical repair of the fracture was planned, using a bioabsorbable screw (Osteotrans-
104 OA²). The screw is made of forged composite materials, which include unsintered
105 hydroxyapatite, embedded in poly L-lactide acid. Since the holding power required
106 for stabilization of a unicortical condylar fracture is likely to be much less than that
107 required for a complete fracture, the authors were confident that this screw would
108 offer adequate mechanical support and chose to take advantage of the
109 osteoconductive, binding and bioabsorbable properties of the composite screw.

110 **2.4 Surgical treatment**

111 The horse was pre-medicated with procaine penicillin 22,000 IU/kg i.m. and flunixin
112 meglumine 1.1 mg/kg i.v. The surgery was performed with the horse conscious,
113 standing, under local analgesia. Detomidine (0.02 mg/kg i.v.) and butorphanol (0.06
114 mg/kg i.v.) were used for sedation. Perineural anaesthesia of the distal limb was
115 performed through a high-4-point nerve block, using a total of 60 ml mepivacaine 2%,
116 [16]. After aseptic preparation of the surgical site, the limb was draped with a sterile
117 sock to accommodate movement during surgery. The site of entrance of the drill bit
118 was identified on dorsopalmar and mediolateral radiographic projections with a
119 hypodermic needle and a stab incision was made in the skin overlying the medial
120 epicondylar fossa. The screw was placed in lag fashion according to the technique
121 recommended by the AO/ASIF. A 4.5 mm glide hole was drilled to just cross the
122 fissure line. A 4.5/3.2 sleeve was inserted to guide a 3.2 mm drill bit, which was used
123 to create the hole across the lateral segment of the bone. The depth of the hole was
124 measured and then the hole was tapped using a 4.5 mm tap. In order to ease the

125 compression between the head screw in the lag hole a countersink was used; then a
126 bioabsorbable screw of 4.5 mm diameter and 50 mm length was inserted (Fig 2A).
127 Bioabsorbable screws are weaker than steel and so particular care was taken when
128 incrementally tightening the screw. In order to achieve optimal compression in an
129 unweighted position, the leg was raised during tightening of the screw (Fig 2B, 2C).
130 Dorsopalmar and mediolateral radiographic projections were performed to assess the
131 position of the screw (Fig. 2E, 2F). The skin was routinely closed with non-
132 absorbable monofilament suture (Ethibond nylon n. 3.5) and the limb was bandaged.

133 **2.5 Post-operative care**

134 The horse was discharged from hospital 24 hours after surgery and antimicrobial and
135 inflammatory treatment (procaine penicillin 22,000 IU/kg i.m. and flunixin
136 meglumine 1.1 mg/kg i.v.) was continued twice daily for 3 days. The bandage was
137 changed every 4 days until suture removal 12 days post-surgery. No complications
138 were observed.

139 **2.6 Outcome and rehabilitation program**

140 After 4 weeks of stall-rest the horse was not lame when examined; thus, a
141 rehabilitation exercise protocol of 15 minutes walking-machine daily for 8 weeks
142 followed by 20 minutes trotting daily for more 6 weeks was scheduled. Radiographs,
143 taken 12 weeks after surgery (Fig 3A) indicated healing of the fracture and no
144 reaction around the screw head. Another MRI examination was performed 18 weeks
145 after surgery, before the horse's workload was increased.

146 **2.7 MRI follow-up**

147 Decrease in the length of the fracture line was associated with resolution of the high
148 intensity signal in the subchondral bone in the STIR sequence. No bone resorption
149 around the screw was apparent (Fig 3B-F).

150 **2.8 Long-term follow up**

151 The horse was monitored closely for one year during which its workload was
152 progressively increased. The horse is free of lameness, the fetlock joint retains full
153 range of mobility and no recurrence of the primary lesion has been observed. The
154 trainer considers that the horse is a “racing prospect”.

155 **2. Discussion**

156 Unicortical condylar fractures are associated with more long-standing, localised bone
157 disease, caused by repetitive stress and, if not recognized, can progress to complete
158 fractures or catastrophic injuries. Unicortical condylar fractures of MCIII/MTIII can
159 be treated conservatively [3,17]. However, cases require stable confinement for at
160 least 8 weeks with or without a cast. Immobilization may decrease bone metabolism,
161 which may also reduce healing process [1,18,19]. The placement of a cortical bone
162 screw in lag fashion to achieve compression across the fracture line will encourage
163 bone healing, leads to a faster recovery of the athletic function, and minimizes the
164 potential risk of re-injury [2,3,5]. Loosening of screws used to stabilize a fracture will
165 result in movement of fragments relative to each other leading to delayed fracture
166 healing. It is essential that the osteosynthesis through internal fixation guarantees a
167 stable interface between fracture margins; moreover, interfragmentary compression is
168 also important in fixation of incomplete fractures [20]. As demonstrated in different
169 studies, the screw used in the present case exhibits an impact strength that increases
170 remarkably between 20-28 weeks compared to the initial values, while it decreases at
171 36 weeks after surgery [7]. The compression strength, calculated as maximum
172 force/compressive area ($S_c = F_{max}/A$), changes least and remains in the region of 110
173 MPa. The compression strength values originate from the compactive polymer which
174 accounts for over 70% of the volume of the composite, while the crystal morphology

175 of multi axial orientation allow remarkably high bending strength [7,20]. Across the
176 fracture line a screw must also provide an initial mechanical bending strength of at
177 least 200 MPa [20], that is higher than natural cortical bone; the bioabsorbable screw
178 used in this report assures a bending strength of 270 MPa for six months [20].
179 Although the aforementioned study was performed on cortical bone of humans [20],
180 other studies about mechanical properties of cortical bones of equine cannon bones
181 showed similar values, with an average bending strength ranging from a median of
182 226 MPa in the lateral and medial quadrants and 195 MPa in the caudal quadrant [21].
183 Moreover, a study reported that the bioabsorbable composite screws stimulate new
184 bone formation 2 weeks after surgery without fibrous tissue formation between bone
185 and screws; it is demonstrated that the surrounding bone directly binds the unsintered
186 hydroxyapatite particles that are partially exposed at the screw surface improving
187 adhesion and osteointegration that are advantageous for initial fracture stabilization
188 [14]. This osteoconductive activity of the bioabsorbable screw may contribute to the
189 early positional stability in the bone [8], and for these reasons they are considered
190 suitable for bone fracture fixation [20]. Several reports in humans demonstrated
191 comparable results in the treatment of ankle fractures and lateral malleolar fractures
192 fixation using unsintered hydroxyapatite/poly L-lactide acid or metallic screws and
193 the time of fracture union were inferior to those of metallic screw [9]. Kuroyanagi *et*
194 *al.* [8] treated tibial condyle fractures in humans, with no breakage of bioabsorbable
195 screws and maintenance of the joint surface at final follow-up in all patients. The
196 histological analysis showed the formation of new bone around the implant at 2
197 weeks; at 8 weeks bone lamellar construction was visible, and at 25 weeks the bone
198 surrounding the composites became normal trabecular bone [8]. The bioabsorbable
199 material gradually deteriorates and the osteoconductivity of unsintered hydroxyapatite

200 promotes the growth of new bone in the region [22]. The absorption mechanism of
201 bioabsorbable screws is not yet fully clarified, certainly it is slow. When it is
202 implanted in the bone, body fluids enter into it via interface between unsintered
203 hydroxyapatite particles and acid matrix reaching the centre of the bioabsorbable
204 screw [22]. The degradation depends on several factors like shape and size of the
205 screw as well as vascularity of surrounding tissue and implantation site [20]. In
206 addition, it is known that the solubility of unsintered hydroxyapatite is enhanced
207 under acid conditions [23]. There is no information about the average time needed to
208 the complete absorption of bioabsorbable screw in horses; it can be assumed that the
209 time required for complete absorption can be similar to that studied in animal models,
210 in which it has taken three years for screws to be phagocytized completely by
211 macrophages [22,24]. The biomechanical trials, the advantages of unsintered
212 hydroxyapatite/poly-L-lactide acid and the proven effectiveness in human long bone
213 fractures repair, have convinced the authors that it was possible to treat unicortical
214 condylar fracture with this specific bioabsorbable screw in horses. While use of
215 conventional metal screws for this surgery is well-established, they do have some
216 disadvantages. For instance, metal screws generate artefacts on computed tomography
217 and MRI and so limit application of these diagnostic modalities post operatively.
218 Furthermore, metal screws sometimes need to be removed which involves a second
219 surgical procedure, with possible complications [6,9]; even when everything goes
220 smoothly, it may sometimes be necessary to remove the screw because its presence
221 reduces the horse value and may prevent the sale. Therefore, the concept behind this
222 surgery is that in selected cases (incomplete fractures) the use of bioabsorbable screw
223 may be beneficial, providing an adequate stabilization and allowing the fracture
224 healing. The MRI, performed 18 weeks after surgery, demonstrated not only bone

225 healing, but most importantly the restoration of more normal bone signal. Although
226 no information about the efficacy of this specific composite screw for fracture fixation
227 in horses is available in the literature, in the present case the fracture line, clearly
228 recognizable on radiographic examination (figure 2B), was no longer visible after
229 screw insertion (figure 2F), suggesting compression through the implant. Moreover,
230 the absence of signs of callus on MRI can demonstrate that a good fracture
231 stabilization was achieved. However, although reports in humans suggests the use of
232 absorbable implants also in displaced fractures [8], it must be taken in consideration
233 that human patients are prohibited from bearing weight for 6 weeks after surgery,
234 which is impossible in horses. For these reasons, bioabsorbable screws are not
235 suitable for unstable or comminuted fractures [20].

236 This study has some limitation; firstly, only one case was included and no comparison
237 with conservative treatment or metallic screw fixation was possible; secondly, the
238 literature available on biomechanical features and the use of this bioabsorbable screw
239 refers to human surgery and/or animal models.

240 **3. Conclusion**

241 To the authors' knowledge, this is the first study reporting outcome of a unicortical
242 condylar fracture treated with a unsintered hydroxyapatite/poly-L-lactide acid screw
243 in a horse. Despite only one horse treated, clinical, radiographic and MRI follow up
244 are encouraging. This kind of screw can be chosen for its mechanical properties, as
245 well as for its osteointegration and osteoinduction capabilities. Further studies are
246 needed; however, bioabsorbable screw offers a promising alternative to treat
247 unicortical condylar fracture and may potentially be used for other orthopaedic
248 surgical treatments as the next-generation material.

249

250 **Manufacturers' address:**

251 ¹Hallmarq Veterinary Imaging Ltd, Unit 5 Bridge Park, Guildford, Surrey, U.K

252 ²Takiron. CO.LTD. Distributor: M.I.T, Localita' I Vaccari, 29122 Piacenza, Italy.

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338

339 **Legend to figures**

340 **Figure 1**

341 A: Flexed dorsopalmar radiographic projection with small radiolucency in medial
342 parasagittal region (red arrow). B-E: MRI transverse STIR-FSE (B-C), T2-FSE (D)
343 and T2-W-FSE (E) sequences through palmar condylar region of the third metacarpal
344 bone showed cortical fissure (red arrow) and extensive signal hyperintensity in the
345 surrounding cancellous bone (yellow arrowheads) of medial condyle. F: T1-W-GRE
346 sequence of sagittal plane, showed extensive signal hypointensity in the surrounding
347 bone (yellow arrowhead).

348 **Figure 2:** Images during surgery.

349 A: Bioabsorbable cortical screw of 4.5 mm diameter diameter composed of
350 hydroxyapatite (HA) and radiolucent poly L-lactide acid (PLLA).

351 B: Dorsopalmar radiographic projection with small radiolucency in medial
352 parasagittal region (yellow arrowhead)

353 C: A 3.2 mm glide hole was created after the fracture line, across the distal cortex.

354 D: The tap is inserted. The condylar fracture is still visible (yellow arrowhead)

355 E: The hole was performed in palmar position.

356 F: The screw was inserted (yellow arrowheads).

357 **Figure 3**

358 A: Dorso-palmar radiographic projection of the metacarpophalangeal joint 12 weeks
359 after surgery.

360 B-E: MRI of the metacarpophalangeal joint in distal-transverse plane STIR-FSE (B),
361 T1-W-GRE (C) and T2-W-FSE (D, E) sequences showed a healing of the condyle
362 fracture with no sclerosis of the surrounding bone. The screw was implanted in
363 palmar position (yellow arrowheads). F: MRI T1-W-GRE sequence of sagittal-lateral
364 plane showed the screw inserted in palmar position (yellow arrowhead), with healing
365 of fracture and no hyperintensity signal around the screw.
366