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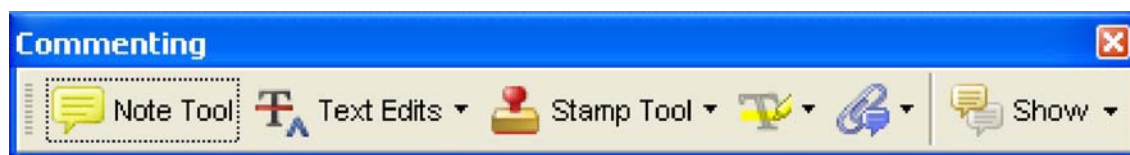
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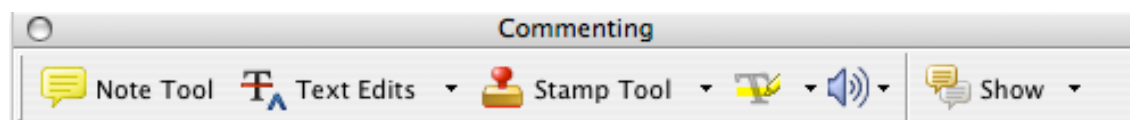
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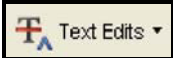
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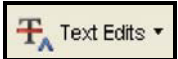
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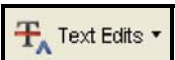
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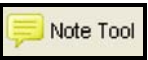
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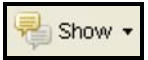
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# Evaluation of Fetal Growth and Fetal Well-Being

Irene Cetin, MD, Simona Boito, MD, PhD, and Tatjana Radaelli, MD

This article reviews the actual knowledge and future developments of ultrasound techniques for the evaluation of fetal growth and well-being. Sonography allows the visualization of the fetus in utero and is utilized worldwide for the evaluation of fetal growth and well-being. Fetal biometry assessment is performed in the second half of pregnancy when deviations of fetal growth can be best recognized through alterations of fetal abdominal circumference growth. Doppler velocimetry of utero-placental vessels identifies alterations of placental perfusion and is valuable in the assessment of fetal brain, heart, and liver perfusion, thus being utilized in the timing of delivery. Recently, three-dimensional ultrasound evaluation of fetal organs and placenta is being developed.  
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Growth of the fetus in utero determines the good outcome of pregnancy, ie, the birth of a healthy and viable child. Normal fetal growth depends on genetic background, endocrine milieu, and the appropriate placental supply of oxygen and nutrients.<sup>1</sup>

Since its introduction into obstetrics in the late 1950s, ultrasound has played an increasingly important role in the characterization of normal fetal growth and the detection of fetal growth abnormalities. Fetal growth assessment is very important to clinicians as decrease or excess in fetal growth is associated with increased mortality and morbidity during the perinatal period<sup>2</sup> and may also be an important antecedent for childhood and adult disease.<sup>3,4</sup>

Improvements in image quality and scanning capability have progressively permitted visualization of greater anatomical detail, which, in turn, has led to more sophisticated analyses of the growth process.<sup>5</sup>

## Fetal Growth and Fetal Well-Being

Changes that influence the supply of nutrients to the fetus might lead to alterations of the fetal growth trajectory. Intra-uterine growth restriction (IUGR) is usually associated with placental insufficiency, while in gestational diabetes mellitus, it has always been hypothesized that excess fetal growth is

deriving from the increased availability of maternal nutrients to the placenta.

Birth weight and gestational age at birth are the most important determinants of neonatal mortality<sup>6</sup> and numerous evidence suggests that low birth weight is associated with the development of the metabolic syndrome.<sup>7</sup>

A strong relationship has been observed between placental weight and birth weight<sup>8</sup> and data arising from large cohort studies have shown that the combination of a large placenta and low birth weight is a strong independent risk factor for cardiovascular disease in adulthood.<sup>9</sup>

The standard curves of birth weight that are commonly used are adjusted for gestational age as well as fetal gender. Other factors have been identified as important in determining birth weight and customized curves have been developed that take into account maternal characteristics such as height, weight, parity, as well as race and ethnic group.<sup>10</sup> Customized birth weight centiles try to assess weight against an individual calculated standard, which is based on the growth potential of each fetus.<sup>11</sup> Adjustments for differences in gestational age and maternal body mass index seem to better predict the SGA-associated risk of perinatal mortality.<sup>12,13</sup>

## Fetal Biometry and Estimation of Fetal Weight

Most ultrasound measurements have been developed with the objective of assessing the size of the fetal trunk and thereby obtaining more accurate information concerning fetal growth.<sup>14,15</sup> Already in 1965 Thompson and coworkers obtained the earliest recorded attempts of fetal cross-sectional area of the trunk.<sup>16</sup> Moreover, trunk measurements have been further developed during the past years and many different techniques have been advocated. These include

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measurements of the thoracic diameters and of the abdominal circumference.<sup>17,18</sup> Measurements of the abdominal circumference at the level of the fetal liver seems to hold the best accuracy and is currently considered an indicator of intrauterine fetal growth in the second half of pregnancy.<sup>19</sup> The rationale for this measurement is that it corresponds most closely with the size of the fetal liver. The work started by Evans and coworkers using an animal model<sup>20</sup> was subsequently confirmed by Gruenwald in the human fetus.<sup>21</sup>

Using ultrasound, other authors<sup>22,23</sup> indicated that the fetal liver is the earliest organ to be affected when intrauterine growth restriction occurs. The detection of fetal growth restriction by means of head circumference measurements in fact may be limited due to fetal brain sparing in the presence of chronic fetal hypoxemia.

An important condition in which we commonly see accelerated fetal growth is maternal insulin-dependent diabetes mellitus. In this clinical condition, fetal biparietal diameter and head circumference measurements conform to normal growth patterns, while growth of the abdominal circumference is abnormally accelerated.<sup>24,25</sup> So far, the ultrasound biometric parameters most commonly used for determining fetal growth are as follows:

- F1 Fetal biparietal diameter and head circumference: these are obtained on a trans-axial section of fetal head that should appear as an oval shape. Landmarks for the right section are the thalamic nuclei and the cavum septi pellucidum (Fig. 1)
- F2 Abdominal circumference: a transverse abdominal section should be obtained including fetal stomach, spine, and deep portion of the umbilical vein (U-shape) (Fig. 2).
- F3 Femur length: measure of the bone diaphysis, excluding distal femoral epiphyses, present after 32 weeks (Fig. 3).

A deeper understanding of fetal growth patterns was reached through customizing the birth weight standard according to physiological variables such as maternal booking weight, maternal height, parity, fetal sex, and ethnic origin.<sup>26</sup>



**Figure 1** Transverse axial sonogram of the fetal head: measurement of biparietal diameter.



**Figure 2** Transverse axial sonogram of the fetal abdomen.

Traditionally, charts of normal fetal biometry have been determined for local populations. As neonatal size was found to vary with the characteristics of the population,<sup>27</sup> these population-based fetal nomograms should be revised regularly, allowing their correct clinical application. In utero fetal growth studies suggested that certain maternal and pregnancy characteristics, such as maternal height and weight, smoking status, ethnic origin, parity, and maternal metabolism, may affect fetal growth.<sup>28,29</sup> Gardosi and coworkers, based on this concept, performed mathematical modeling in which the effects of pregnancy characteristics to produce a customized birth weight standard were taken into account.<sup>11</sup> Since birth weight is regarded as an outcome measure of fetal growth, assessment of fetal growth in utero appears to be helpful in making clinical management decisions in very low birth weight or large babies. With modern sonographic technology, fetal weight can be estimated with reasonable accuracy.<sup>30,31</sup>

The most successful early approach to estimate fetal weight was a simple correlation between abdominal circumference and birth weight.<sup>17</sup> Numerous further attempts have com-



**Figure 3** Longitudinal sonogram of the fetal femur length.



110 bined measurements in regression equations or volumetric  
 111 formulae with different degrees of accuracy. Several of these  
 112 methods have insignificant systematic errors, but random  
 113 errors (ie, standard deviation of errors) of less than 7% are  
 114 rarely reported. The accuracy of estimated fetal weight is also  
 115 compromised by large intra- and interobserver variability.<sup>32</sup>  
 116 Many regression formulae for sonographic fetal weight esti-  
 117 mation have been published during the last 30 years, which,  
 118 unfortunately, generally show poor rates of accuracy. Com-  
 119 monly used formulae in different birth weight groups were  
 120 recently compared to assess whether any of the formulae are  
 121 more or less favorable.<sup>33</sup> Over the whole weight range and in  
 122 the subgroup of newborns with a birth weight less than  
 123 2500 g, two Hadlock regression formulae (including abdomi-  
 124 nal circumference, femur length, biparietal diameter with or  
 125 without head circumference) showed the best levels of accu-  
 126 racy. Infants with a birth weight between 2500 and 3999 g  
 127 and >4000 g were best estimated using the gender-specific  
 128 Schild formula (different formulae for girls and boys)<sup>34</sup> and  
 129 the Merz's regression formula, respectively.<sup>35</sup>

130 In summary, although ultrasound has been shown to be an  
 131 invaluable tool for the assessment of fetal growth patterns,  
 132 the measurements currently employed are less than ideal,  
 133 since mathematic formulas are necessary to convert them  
 134 into weight or volume.

135 Moreover, no significant differences were observed in a  
 136 recent study when comparing clinical versus sonographic  
 137 estimation of fetal weight in the normal weight range, except  
 138 that, while the ultrasonographic method underestimated  
 139 birth weight, the clinical method overestimated it. Moreover,  
 140 ultrasound demonstrated more accurate compared to the  
 141 clinical evaluation in detecting low-birth-weight babies.<sup>36</sup>

142 **Evaluation of Fetal Body Composition**

143 Fetal body composition changes throughout gestation. Spe-  
 144 cifically, a large and exponential deposition of fat tissue oc-  
 145 curs during the second half of gestation, when most of fetal  
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**Figure 4** Fat mass measured at the level of middle arm: the measure was obtained as the difference between total arm area and lean mass area (muscle and bone).



**Figure 5** Abdominal fat thickness measured at the level of abdominal circumference.

125 weight is gained.<sup>37</sup> Fetal fat mass growth seems to better  
 126 correlate with the intrauterine environment, whereas fat-free  
 127 mass shows stronger relationships with genetic factors. This  
 128 is supported by evidence showing that the differences in  
 129 weight at birth of babies born small or large for gestational  
 130 age are due to the different percentage of fat at birth, repre-  
 131 senting up to 46% of the variance in neonatal weight.<sup>38,39</sup>

132 Anthropometric ultrasound measurements of fetal body  
 133 composition of normal fetuses have shown a unique expo-  
 134 nential pattern of the growth profile during the second half of  
 135 gestation both in lean mass and in fat mass.<sup>40</sup> Fat and lean  
 136 mass can be measured at the level of the thigh and the arm  
 137 (Fig. 4). Moreover, subcutaneous fat can be measured as  
 138 subcutaneous abdominal fat thickness (Fig. 5) and subscap-  
 139 ular fat thickness. Although alterations of fetal growth trajec-  
 140 tory are associated with decreased abdominal circumference  
 141 measurements, fetal biometry has limitations in differentiat-  
 142 ing the growth-restricted fetus from a fetus that is constitu-  
 143 tionally small. Reduced subcutaneous fat mass has been  
 144 shown in IUGR fetuses and the reduction is more significant  
 145 when fat is normalized for body size.<sup>41</sup> On the other hand, in  
 146 gestational diabetes mellitus the increased intrauterine  
 147 growth is reflected in increased fetal fat mass deposition<sup>42</sup>  
 148 and intrauterine ultrasound evaluation of fetal fat correlates  
 149 with fetal leptin levels.<sup>43</sup>

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**Three-Dimensional Ultrasound in the Evaluation of Fetal Weight and Fetal Organ Volumes**

161 With the introduction of three-dimensional (3D) sonography  
 162 at the beginning of the 1990s, reproducible circumference  
 163 and volumetric measurements have become feasible by si-  
 164 multaneous visualization of three orthogonal fetal sections  
 165 and volume calculation has been considerably simplified.<sup>44,45</sup>  
 166 Three-dimensional ultrasonography allows assessment of the  
 167 shape and volume of fetal organs.<sup>46-48</sup>

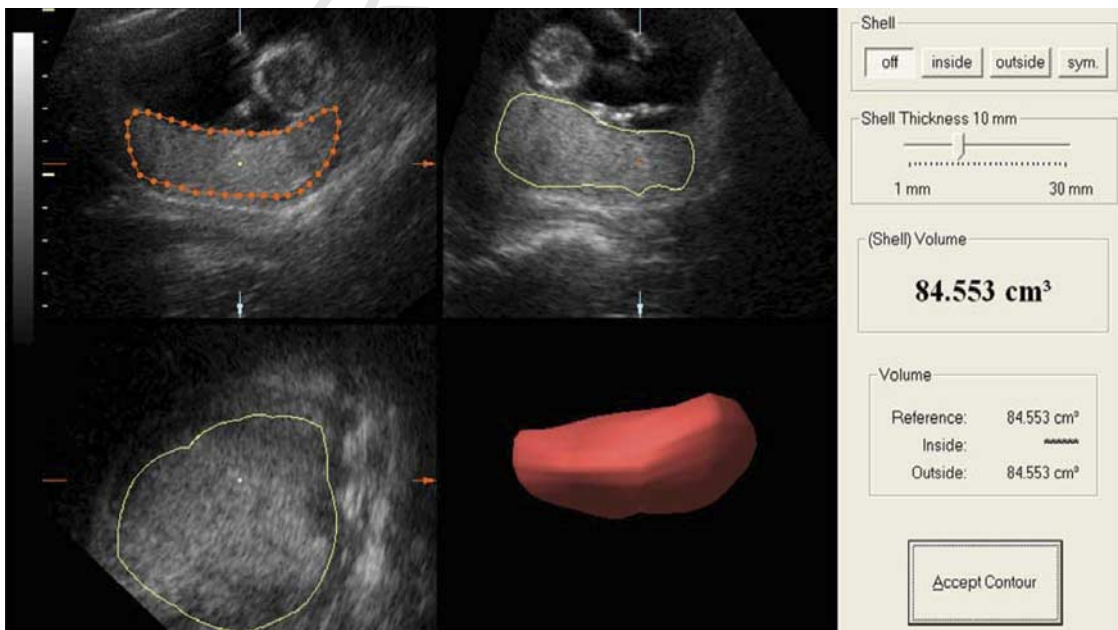
### 3D Ultrasound Technique

The three-dimensional ultrasound technique uses computer processing for 3D reconstruction. A consecutive set of two-dimensional (2D) planes is acquired by movements of the ultrasound probe (free hand or mechanically) and constructed into a 3D data set by a computer. By using a position sensor or electromagnetic sensing device, the position of every pixel of 2D images within the volume is determined and 3D reconstruction can be built. The 3D ultrasound machine commonly used is equipped with an automatic volume scanning method. The ultrasound probe has a built-in mechanical device to move the transducer along with a position sensor. The patient setting of a 3D ultrasound examination is identical to that of a conventional 2D ultrasound examination. Orientation with real-time 2D ultrasound and optimization of the B-mode image (the normal 2D ultrasound mode) is necessary before 3D acquisition can take place. Acquisition is performed automatically after the examiner defines a region of interest (the so-called "volume box"). The digitized information of every section plane is loaded into a computer along with the information regarding its position. The 3D data set is thus composed of a set of voxels, each with a certain gray value and brightness. These values are interpolated to the voxels in-between two section planes.<sup>47-49</sup> After acquisition, three orthogonal planes in the direction of three orthogonal axes (*x*; *y*; *z*) are displayed on the monitor (multiplanar view) (Figs. 6 and 7). These planes can be moved and rotated freely with an automatic update of the perpendicular planes. 3D image reconstruction takes place after a box is set around the region of interest within the volume, thus extracting unwanted parts.

### Liver Volume

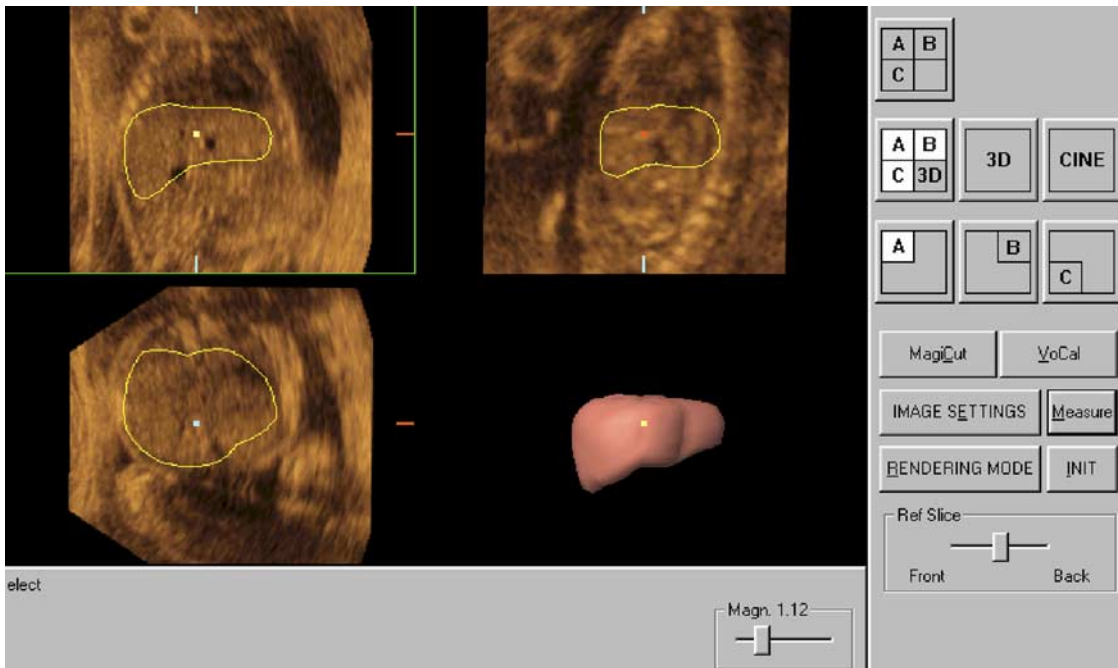
As already discussed, numerous studies have shown that the most effective method of detecting impaired fetal growth is the sonographic measurement of the upper abdominal circumference.<sup>50,51</sup> However, this measurement is not completely satisfactory in that the positive-predicted value for detecting fetal growth restriction may be as low as 21%.<sup>52</sup> The fetal liver comprises most of the abdomen measured by the abdominal circumference, and changes in fetal liver weight are strongly associated with induced intrauterine growth restriction in animals.<sup>1</sup> Moreover, reduction in fetal liver weight is more pronounced than reduction in brain weight due to the brain-sparing effect, reflecting redistribution of fetal blood flow during chronic fetal hypoxemia.<sup>53</sup>

The reproducibility of fetal liver volume recordings and tracings has been shown to be quite accurate with a total coefficient of variation of less than 4%.<sup>54</sup> In uncomplicated pregnancy, fetal liver volume demonstrates a 10-fold increase with advancing gestational age (Fig. 8) and increasing fetal weight. The regression line, shown in Figure 9, demonstrates that the liver volume is proportional to estimated fetal weight during the second half of pregnancy. Fetal growth restriction is associated with reduced liver volume in every instance. When looking at the mean difference in liver volume between normal and reduced fetal growth, as expressed by the Z-score, a significant difference is confirmed when compared with the head circumference, confirming the brain-sparing effect during abnormal fetal development. It can be concluded that liver size is affected in fetal growth restriction, but fetal liver volume measurement is not a better discriminator than measurement of the upper abdominal circumference.



**Figure 6** Placental volume calculations and the final three-dimensional image of the placenta. (Color version of figure is available online.)





**Figure 7** Liver volume calculations and the final three-dimensional image of the fetal liver. (Color version of figure is available online.)

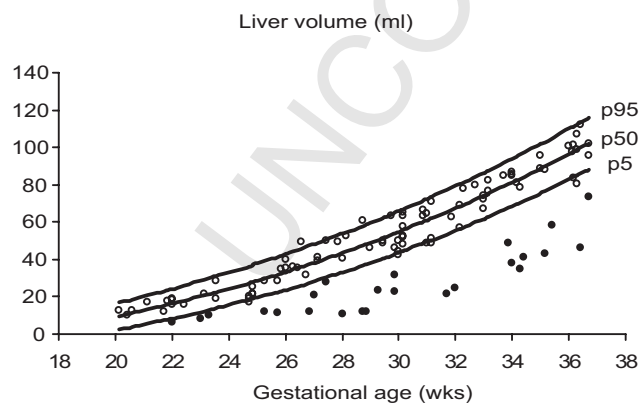
### Brain Volume

Both fetal biparietal diameter and fetal head circumference are standard parameters in establishing normal and abnormal fetal biometry.<sup>14</sup> With the use of a 3D sonographic method, it is now possible to measure fetal brain volume with an acceptable intraobserver variability. A nearly 10-fold increase in fetal brain volume takes place during the second half of gestation. At the same time brain growth demonstrates a marked slow down as expressed by a weekly increment in brain volume at 34 weeks of only one-third of the weekly increment at 19 weeks of gestation. When fetal brain weight derived from

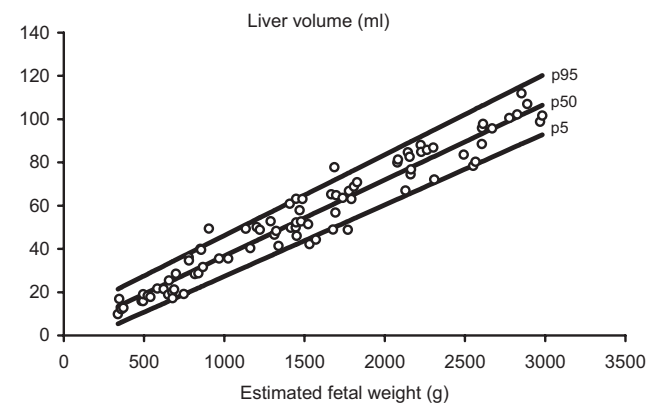
brain volume is examined, this represents 14 to 17% of total estimated fetal weight. Fetal brain volume measurement in conjunction with fetal liver volume determination could provide insight into the nature of abnormal fetal growth.

### Brain Liver Volume Ratio

Post-mortem studies have established that fetal growth restriction is associated with an increased brain/liver volume ratio. During fetal hypoxemia, reduction in fetal brain weight is less pronounced than fetal liver weight and this phenomenon is caused by fetal circulatory centralization and fetal



**Figure 8** Liver volume (milliliters) relative to gestational age (weeks). The figure shows that all liver volumes of the growth-restricted fetuses are situated below the P5 reference level. Open circles (O) represent individual normal values; solid line (—): P5, P50, and P95 reference lines. Closed circles (●) represent fetal growth restriction. GA = gestational age. P50: cubic fit =  $0.0012 \times GA^3 + 0.0443 \times GA^2 - 18.268$ . P5-P95 =  $P50 \pm 1.64 (-0.2408 \times GA - 0.4560)$ .



**Figure 9** Liver volume (milliliters) relative to estimated fetal weight (grams). The regression line demonstrates that the liver volume is proportional to estimated fetal weight during the second half of pregnancy. Open circles (O) represent individual normal values; solid line (—): P5, P50, and P95 reference lines. Estimated fetal weight. P50: linear fit =  $35.190623 \times EFW + 1.560381$ . P5-P95 =  $P50 \pm 1.64 (1.300713 \times EFW + 4.447085)$ .

brain sparing, resulting in asymmetrical growth restriction. Using 3D ultrasound scanning a mean brain/liver volume ratio of 3 was found in normal developing pregnancies and a maximum value of 10 has been reported in IUGR fetuses.<sup>55</sup> These measurements indicate the possibility of calculating fetal brain/liver volume ratio as a tool to monitor fetal growth restriction, and to indirectly indicate fetal hypoxemia. It thus becomes of interest to evaluate how this ratio relates to umbilical venous volume flow, responsible for oxygen transfer to the fetus. An inverse relation has been found in the growth-restricted fetus between fetal brain/liver volume ratio and fetal weight-related umbilical venous blood flow. Raised fetal brain/liver volume ratios were first found at reduced fetal weight-related umbilical venous volume flows of 70 ml/min/kg, and an average gestational age of 30 weeks.<sup>55</sup>

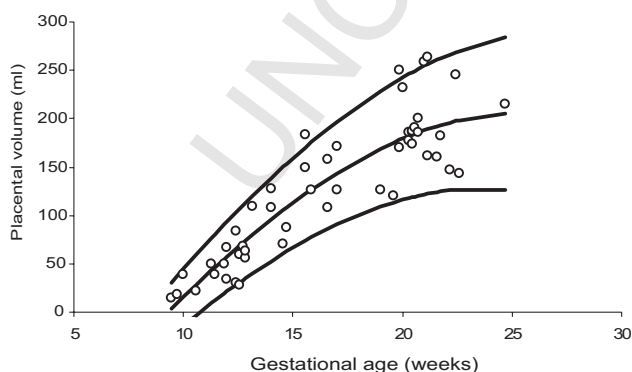
## Placental Volume

Ultrasound is the most sensitive and less invasive method to evaluate placental size and morphology. The three-dimensional approach allows the calculation of placental volume in the first and second trimester of pregnancy. Intra- and inter-observer reproducibility of placental volume measurements was tested showing a good reproducibility.<sup>56</sup> Reference values for placental volume in normally developing fetuses have been established during the first half of pregnancy according to a cross-sectional study design (Fig. 10).<sup>56</sup> Mean placental volume (P50) ranged between 15.8 ml at 10 weeks and 198.4 ml at 23 weeks. A positive correlation existed between placental volume and fetal biparietal diameter ( $r = 0.81$ ). Normal placental volume is 12-fold larger at midgestation compared with the beginning of pregnancy, confirming that placental growth occurs mainly in the first half of pregnancy.

## Doppler Velocimetry: Profiles and Estimation of Flows

### Uterine and Umbilical Blood Flow Profiles

Uterine blood flow provides oxygen and nutrient supply to the placenta and to the fetal circulation. During normal preg-

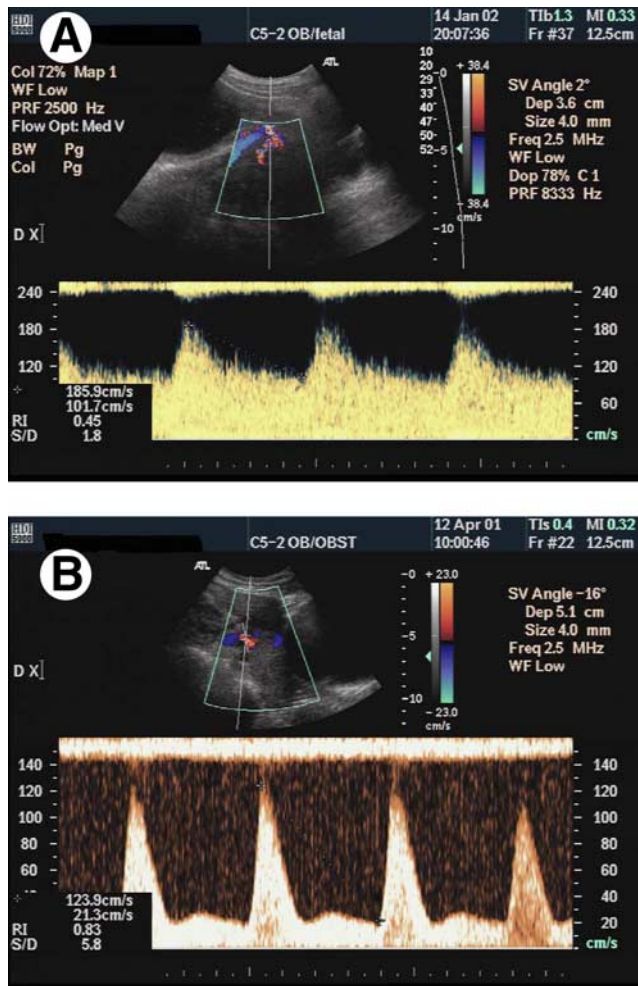


**Figure 10** Placenta volume (milliliters) relative to gestational age (weeks). Open circles (O) represent individual normal values; solid line (—): P5, P50, and P95 reference lines. P50: cubic fit =  $-228.75 + 25.8124 \times (\text{gestational age}) - 0.0135 \times (\text{gestational age})^3$  P5-P95 =  $P50 \pm 1.645 \times 1.25 \times (-1.9685 + 1.6315) \times (\text{gestational age})$ .

nancy, deep anatomic and functional changes occur in the utero-placental circulation. Between 10 and 24 weeks of gestation, two subsequent trophoblast migration waves into spiral arteries wall lead to a larger lumen diameter and a total lack of wall arterial elasticity. Spiral arteries progressively become low wall resistance vessels, allowing the physiological increase of blood flow into the intervillous space. Adequate placentation is essential to guarantee a normal obstetric outcome. Doppler studies show vessel remodeling is rapid, with the loss of proto-diastolic notching by 12 weeks and low resistance indices by 20 weeks or sooner.<sup>57,58</sup> On the contrary, when placentation is deficient (incomplete/absent trophoblast migration into arteries wall), notching remains, and high resistance may persist even after 24 to 26 weeks; pregnancy is associated with a significantly higher risk of both maternal (gestational hypertension, preeclampsia) and fetal diseases (intrauterine growth restriction). Uterine artery Doppler velocimetry represents the gold standard to screen and to diagnose placental defects in at-risk pregnancies. In these pregnancies the utero-placental circulation remains in a state of high resistance, which may cause generalized endothelial cell injury, compromising vascular integrity and an atherosclerosis-like process with consequent small-vessel occlusion, local ischemia, and necrosis.<sup>59</sup> This condition can be noninvasively evaluated by Doppler ultrasound<sup>60</sup>: uterine artery Doppler measurements show that impedance to flow in the uterine arteries (ie, Resistance Index or S/D ratio) decreases with gestational age in normal pregnancies (Fig. 11A). On the contrary, impedance to flow is increased in established preeclampsia and IUGR<sup>61</sup> (Fig. 11B). A correlation between qualitative and semi-quantitative Doppler indices and histological placental lesions has been consistently reported.<sup>62-65</sup> There have been a number of studies that have examined the ability of uterine artery Doppler velocimetry to predict complications of impaired placentation.<sup>66</sup> Most studies have used uterine artery Doppler in the second trimester showing detection rates of 80 to 90% for early onset preeclampsia (requiring delivery before 34 weeks), but only of 41 to 45% for preeclampsia at any gestational age, with false-positive rates between 5 and 7%.<sup>67</sup> Using first-trimester screening shows a similar trend, although overall detection rates are lower than screening in the second trimester.<sup>68,69</sup>

## Fetal Circulation

Umbilical artery is the first and most studied vessel in obstetrics. Doppler study of umbilical artery is not time consuming and can be done with any Doppler system, with or without the support of B-mode real-time ultrasound image. In the assessment of blood flow characteristics of the umbilical artery, any index (S/D ratio, Pulsatility Index, or Resistance Index) has been found to be accurate.<sup>60</sup> Pulsed Doppler assessment of the umbilical artery blood flow in ongoing pregnancy is characterized by low-resistance blood flow pattern with high velocities in both systolic and diastolic phase of the cardiac cycle, but this varies with gestation. End-diastolic velocity in the umbilical artery is the result of the placental resistance. In early normal pregnancy, when the placenta is



**Figure 11** Uterine artery Doppler measurements showing in (A) normal waveform with Resistance Index and S/D ratio within normal ranges. (B) A blood flow profile typically present in pregnancies complicated by preeclampsia or IUGR: RI and S/D ratio are increased and a proto-diastolic notch is well documented. (Color version of figure is available online.)

still a high resistance unit, decreased or absent end-diastolic velocity are probably normal, but successful placental invasion leads to falling resistance and continuous diastolic flow in the umbilical artery Doppler by 14 to 18 weeks at the latest<sup>70</sup> (Fig. 12). A continuous decline in umbilical artery resistance over gestation closely correlates with normal birth weight, low risk of fetal distress, neonatal complications, and longer term manifestations of placental deficiency.<sup>71</sup> Conversely, rising resistance and severity of changes in Doppler velocimetry, with progression to the loss and eventually the reversal of end-diastolic flow, significantly correlates with worse perinatal outcome<sup>72</sup> (Fig. 13). Despite this evidence, current fetal surveillance and timing of delivery are primarily based on changes observed in the fetal heart recording (FHR). However, when FHR tracing has become abnormal, up to 77% of IUGR fetuses are already hypoxic and acidemic.<sup>73</sup>

Recent technological advances in ultrasound and Doppler imaging have permitted detailed examination of fetal vessels

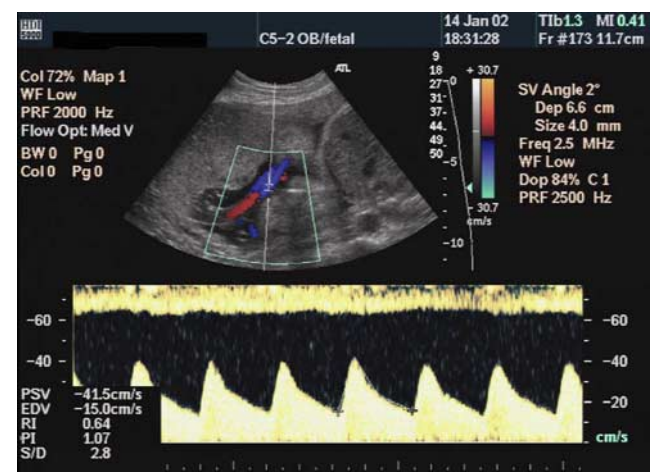
in the peripheral and central circulations. Fetal hypoxia and acidemia have been found to be associated with abnormal velocimetry of the middle cerebral artery, the aorta, the inferior vena cava, and the ductus venosus, demonstrating preferential blood flow to the brain and myocardium, and reduced perfusion to the splanchnic organs.<sup>74</sup> The increased frequency of intraventricular hemorrhage in decreased or absent end-diastolic velocity/REDV IUGR babies offers specific evidence of the role of the brain-sparing effect.<sup>75</sup> Worsening flow in the umbilical artery and persistent dilatation of the middle cerebral artery can be defined as early stage modifications, being present 2 to 3 weeks prior to any changes in the FHR tracing in more than 50% of IUGR fetuses.<sup>74</sup>

While arterial waveforms describe downstream resistance in critical vascular beds, venous Doppler provides important data about cardiac function. Among the studied veins, the inferior vena cava has a wide variation within normal fetuses,<sup>76,77</sup> and the umbilical vein has an irrelevant sensitivity despite a very specific indication of stillbirth risk, resulting in a very low predictive value for asphyxia, or even stillbirth.<sup>78</sup>

The ductus venosus provides a unique combination of advantages, being a primary regulator of venous return in both normal and abnormal fetuses, and being responsive to changes in oxygenation, independent of cardiac function. Moreover, although all studied venous vessels provide a valuable correlation with fetal and neonatal morbidities, the retrograde ductus venosus atrial-wave is the simplest to recognize and is the best predictor of perinatal mortality, neonatal circulatory collapse, and other critical morbidities.<sup>79</sup>

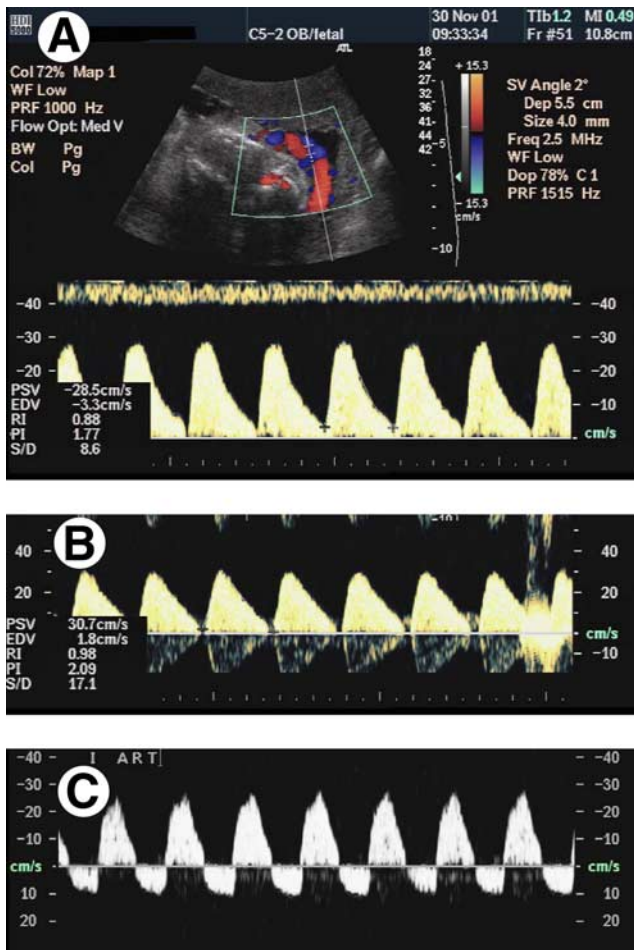
### Sequence of Doppler Velocimetry Profile Changes in IUGR

The pathophysiology of intrauterine growth restriction has been investigated in numerous studies that have led to the characterization of a specific placental phenotype leading to reduced nutrient transfer followed by placental respiratory



**Figure 12** Umbilical artery Doppler waveform: presence of continuous diastolic flow in the umbilical artery of a normal fetus. All impedance indices (PI, RI, and S/D ratio) decrease with gestation, representing a decrease in placental vascular resistance. (Color version of figure is available online.)





**Figure 13** Increased placental vascular resistance correlates with worst perinatal outcome. IUGR fetuses show progressive worsening of the waveform with a reduction (A) and the loss of end-diastolic flow (B) until the reversal of end-diastolic flow (REDF) (C). (Color version of figure is available online.)

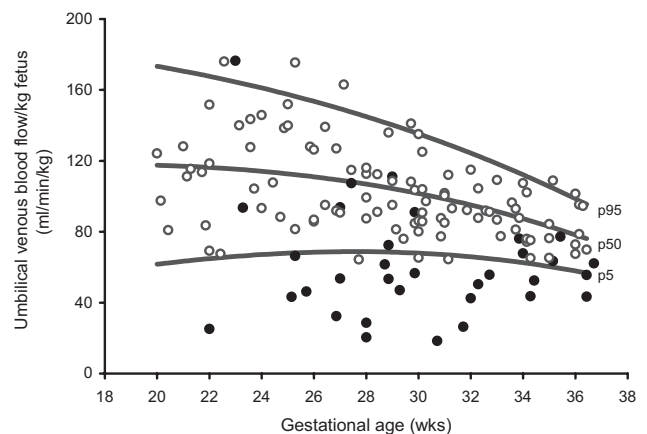
failure and fetal hypoxemia.<sup>80,81</sup> A temporal sequence of events has been described in the fetus indicating (1) reduction of growth under normoxic conditions, followed (2) by an adaptation phase with compensatory hemodynamic changes, which include blood flow redistribution towards essential organs such as the brain, heart and adrenal gland at the expenses of other organ systems (liver, lungs, kidneys, bowel).<sup>74</sup> This phenomenon is the so-called “centralization” of the fetal circulation. This compensatory phase of the disease can be recognized clinically by typical Doppler ultrasound findings, including a decrease in the pulsatility index of the middle cerebral artery, a decrease in the amniotic fluid, and by increased echogenicity of the bowel. The duration of this compensatory phase is variable, sometimes lasting weeks, and appears not to have deleterious short-term consequences, although it is likely to be associated with changes in fetal programming potentially associated with increased likelihood of long-term consequences.<sup>82</sup> When the adaptation phase with these compensatory mechanisms reach their limit, (3) myocardial dysfunction occurs.

At this time, hemodynamic decompensation is clinically recognized by abnormal venous Doppler waveforms, which are considered to reflect increased pressure in right atrium and/or dilatation of the DV and are often associated with metabolic acidemia.<sup>83</sup> Hypoxemia and acidemia have been well described to occur significantly only in this phase and are associated to abnormal fetal heart rate tracings.<sup>73</sup> Once the disease enters this decompensatory phase, the fetus is at high risk of dying and of developing multisystem organ failure.<sup>84</sup>

### Estimation of Umbilical Venous Volume Inflow

Until recently, evaluation of the umbilical venous circulation has evoked only limited interest in favor of the umbilical artery circulation. Few data have appeared on volume flow due to the lack of precision of components measurements, notably cross-sectional vessel size. By means of a method that allows accurate determination of umbilical venous cross-sectional area, it has become possible to obtain a full picture of the clinical significance of subsequent volume flow calculations in the human fetus. Umbilical venous volume flow demonstrates no differences at the fetal, placental, or free loop site of the umbilical cord.<sup>85</sup> Normal mean umbilical venous blood flow ranges between 33 ml/min at 20 weeks and 220 ml/min at 36 weeks, which is a sevenfold increase.<sup>54</sup> When calculated per kilogram fetus as shown in Fig. 14, there is a significant decrease in normal volume blood flow from 117.5 ± 33.6 ml/min at 20 weeks to 78.3 ± 12.4 ml/min at 36 weeks of gestation.

The sevenfold increase between 20 and 36 weeks in umbilical venous volume flow has been established under physiological circumstances and is mainly determined by an increase in cross-sectional vessel size, with a significant



**Figure 14** Umbilical venous volume flow/kg estimated fetal weight (ml/min/kg) relative to gestational age (GA). Open circles (○) represent individual normal values; solid line (—): P5, P50, and P95 reference lines. Closed circles (●) represent fetal growth restriction. GA = gestational age. P50: cubic fit =  $-0.001670 \times GA^3 + 1.579665 \times GA + 99.293341$ . P5-P95 =  $P50 \pm 1.64 (1.076244 \times GA + 48.623154)$ .

reduction in fetal weight-related umbilical venous volume flow.

Fetal growth restriction is associated with significantly lower umbilical venous volume flows, which again is mainly determined by a reduction in cross-sectional vessel size.<sup>54</sup> In this condition, umbilical artery Pulsatility Index reflecting fetoplacental downstream impedance is significantly raised when fetal weight-related umbilical venous volume flow is below the lower limit (5th centile) of the normal range compared with normal values.

### Estimation of Uterine Artery Volume Flow

Quantitative information of the utero-placental blood volume flow can widely improve our knowledge on utero-placental vascularization throughout gestation. However, up to now, despite extensive clinical use of uterine Doppler waveform analysis, only few studies have proposed methods to quantify the blood volume flow through uterine arteries and a correlation between flow and resistance Doppler indices in these vessels has never been described. Our group recently reported preliminary data of a mean uterine blood flow volume of 237.8 ml/min (range, 94 to 654.5 ml/min) at mid gestation.<sup>86</sup> These values indicate that, in normal pregnancy at mid gestation, there is a great variability in the amount of blood flow volume that supplies placental tissue. This uterine flow volume redundancy seems to remain stable up to term, since the uterine flow volume in the third trimester is 528.9 ml/min (range, 201.9 to 1471.4 ml/min) and does not seem related to side of placental insertion.

### Conclusions

Ultrasound has become an invaluable tool in obstetrics that has made possible to both clinicians and parents knowledge of the fetus while in the mother's womb. Fetal growth and well-being can be evaluated by traditional fetal biometry assessment performed in the second half of pregnancy. Moreover, when deviations of fetal growth are recognized, Doppler velocimetry of utero-placental and fetal vessels is utilized in the timing of delivery. New technologies are now being studied to better describe fetal body composition and development of fetal organs.

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